

Seventeen Years of Functional MRI

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Laboratory of Brain and Cognition

<http://fim.nimh.nih.gov>

&

Functional MRI Facility

<http://fmrif.nimh.nih.gov>



1. A bit of history of MRI
and functional MRI

2. Basics of functional MRI
contrast and methods

3. Basic and cutting edge
applications

Magnetic Resonance Imaging

1984

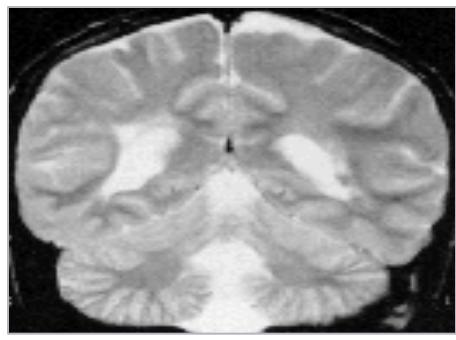


Water: 42 MHz/Tesla

1.5 Tesla = 63 MHz

3 Tesla = 126 MHz

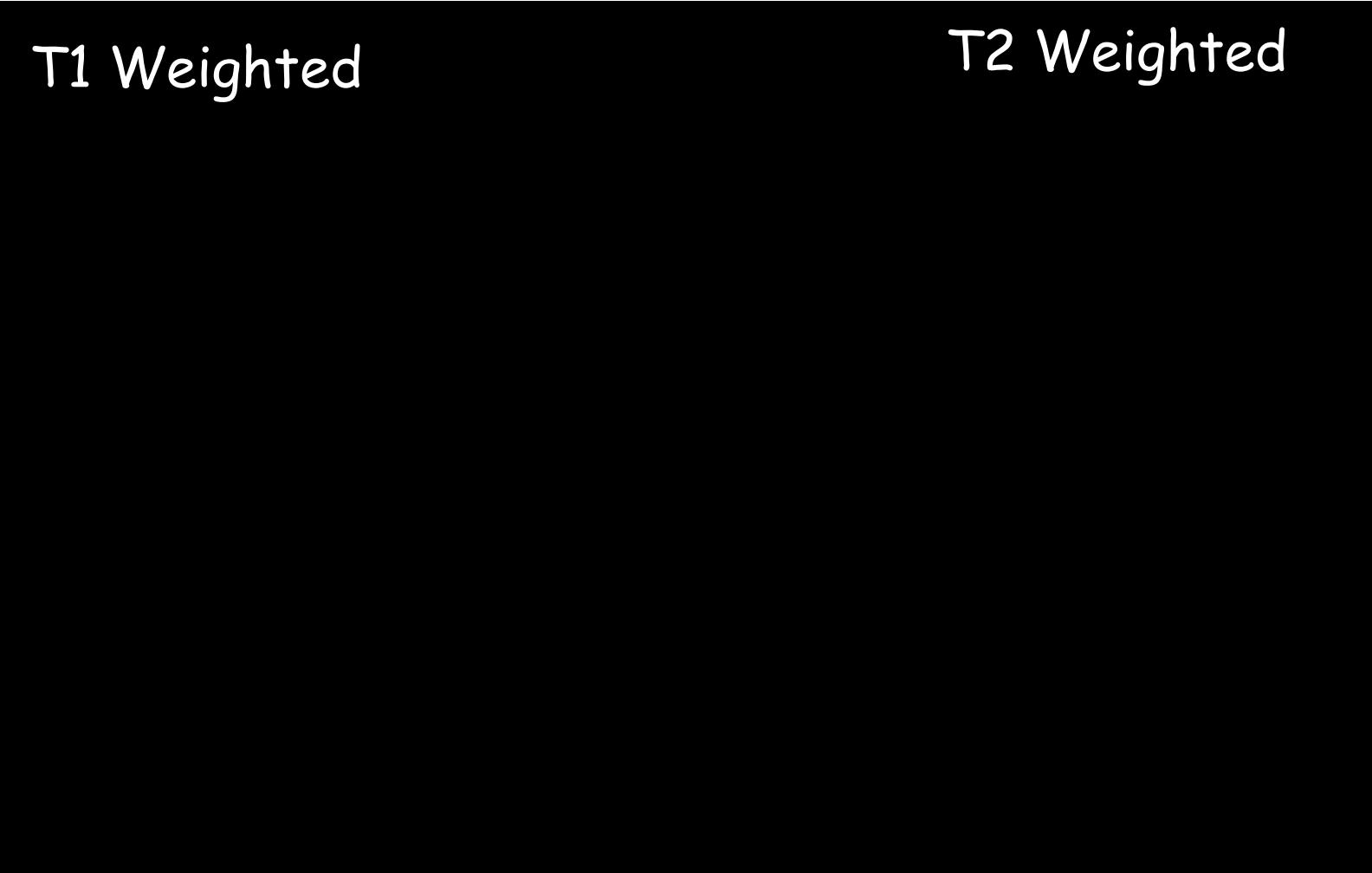
7 Tesla = 294 MHz



MRI Images with Different Contrast Weighting

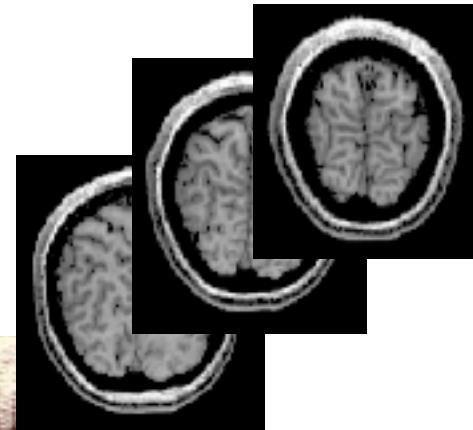
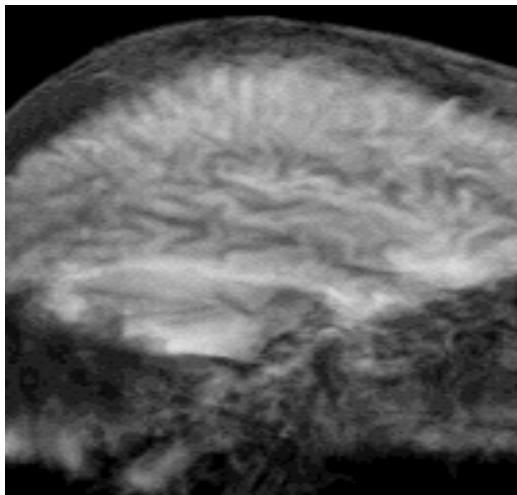
T1 Weighted

T2 Weighted



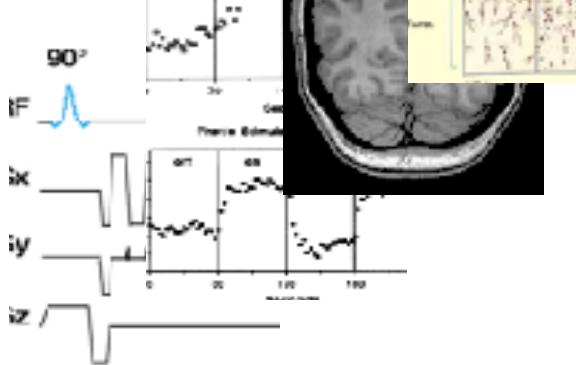
Venography

Fiber Track Imaging



Anatomy

Angiography



Perfusion



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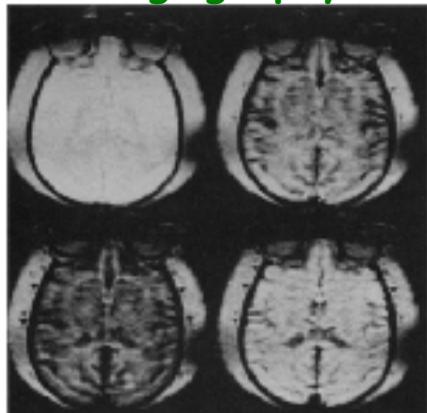
3. Basic and cutting edge
applications



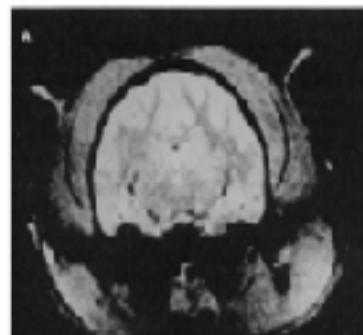
metabolic imaging (NAA)

(1990) *Science*, 250, 53-61.

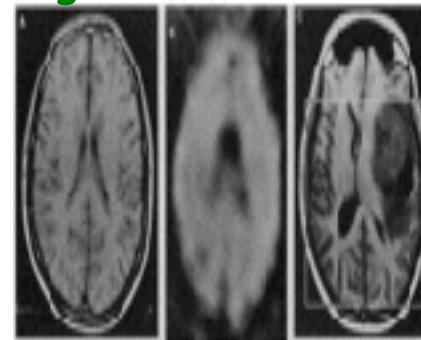
angiography



Diffusion



magnetization transfer



Gadolinium perfusion

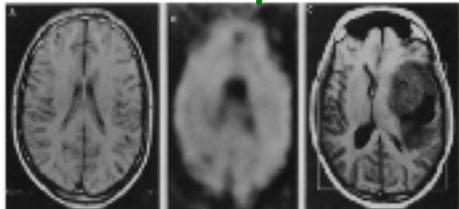


Fig. 7 Immunofluorescence of *Leishmania* in macrophages. Cells were infected with promastigotes of *L. mexicana* and examined at day 10 post-infection. Control cells were infected with heat-killed promastigotes. *L. mexicana* was used in many studies as the model parasite for the study of Leishmaniasis. In this example, we can see the intracellular parasites in control cells and the absence of parasites in heat-killed cells. The *L. mexicana* parasites were visualized by the antibody directed against the protein of 60 kDa. The 60 kDa protein of these parasite is a major antigenic component of the parasite. The immunofluorescence technique is a good method to study the intracellular parasites. The fluorescence images are good to study the localization of the parasite in the host cell. After the infection, the parasites are taken up by the host cell and are localized in the cytoplasm. After the infection, the parasites are taken up by the host cell and are localized in the cytoplasm. The fluorescence images are good to study the localization of the parasite in the host cell.

NAA

choline

creatine lactate

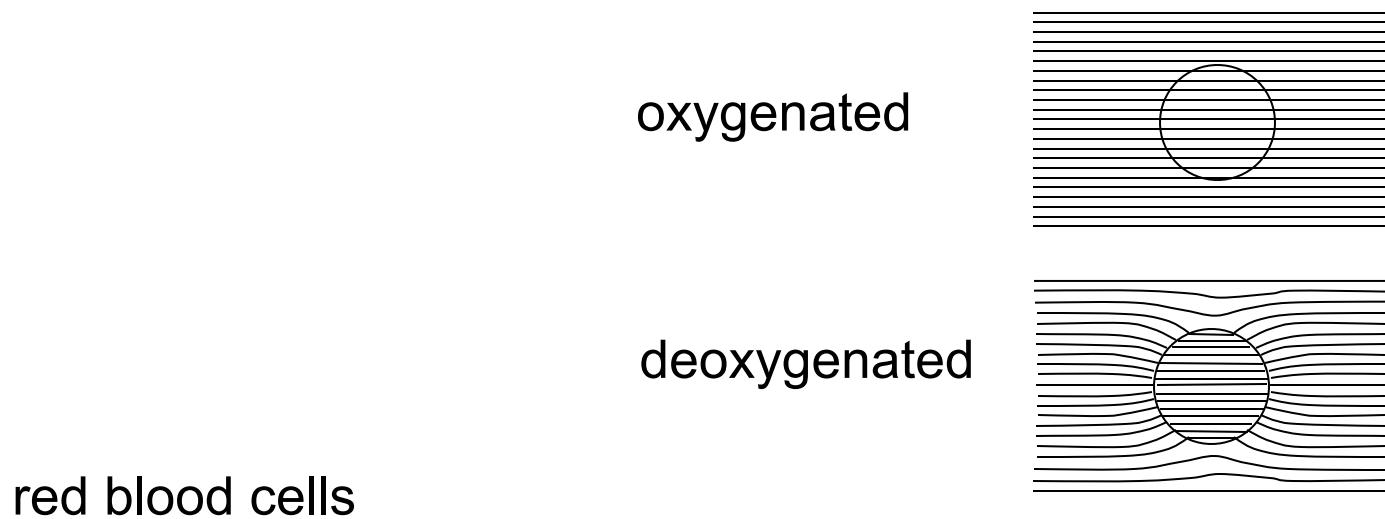
Magnetic Properties of Blood

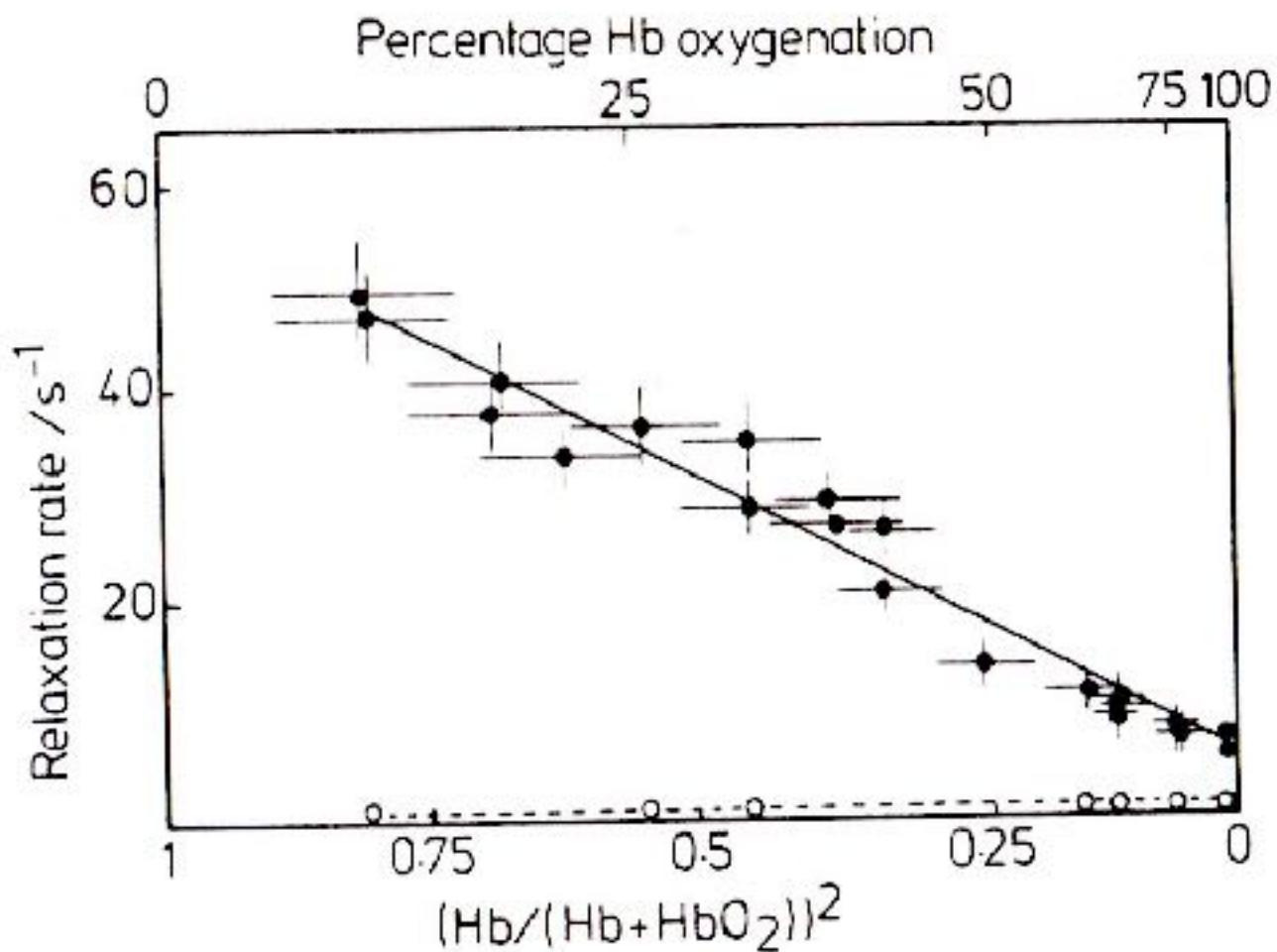
L. Pauling, C. D. Coryell, Proc.Natl. Acad. Sci. USA 22, 210-216, **1936**.

K.R. Thulborn, J. C. Waterton, et al., Biochim. Biophys. Acta. 714: 265-270, **1982**.

S. Ogawa, T. M. Lee, A. R. Kay, D. W. Tank, Proc. Natl. Acad. Sci. USA 87, 9868-9872, **1990**.

Turner, R., Lebihan, D., Moonen, C. T. W., Despres, D. & Frank, J. Magnetic Resonance in Medicine, 22, 159-166, **1991**.

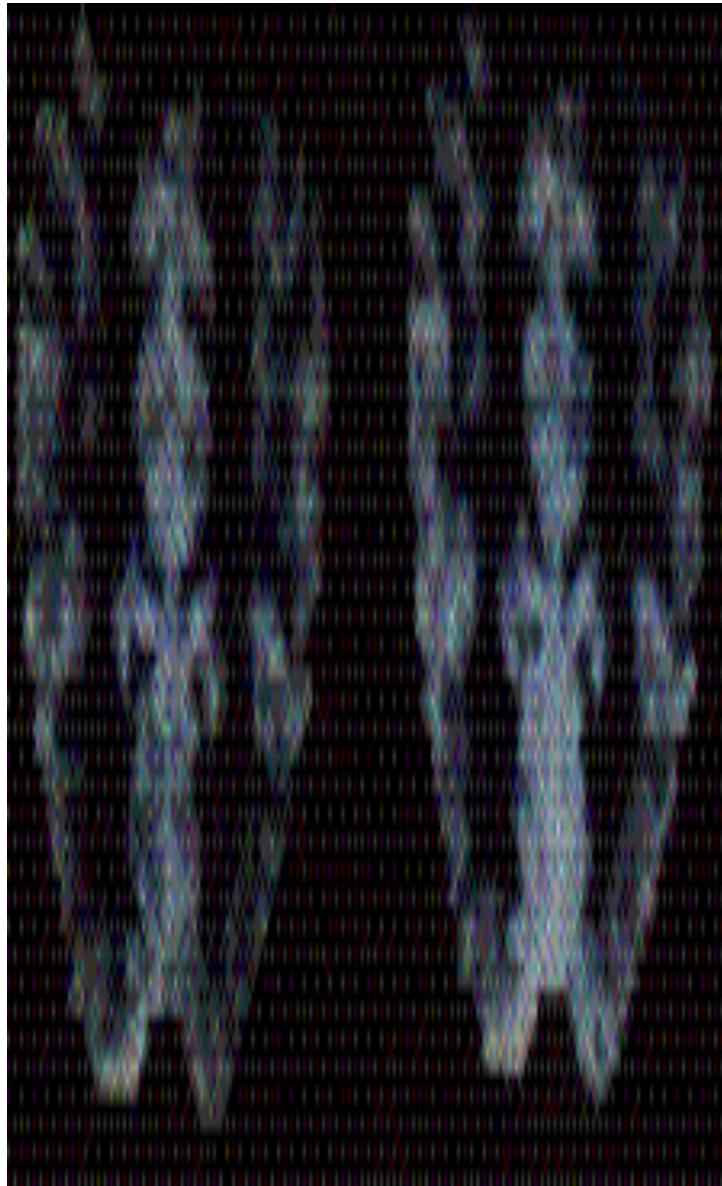




K. R. Thulborn, J. C. Waterton, P. M. Matthews, G. K.
Radda, Biochimica et Biophysica Acta, 714, 265-270, 1982

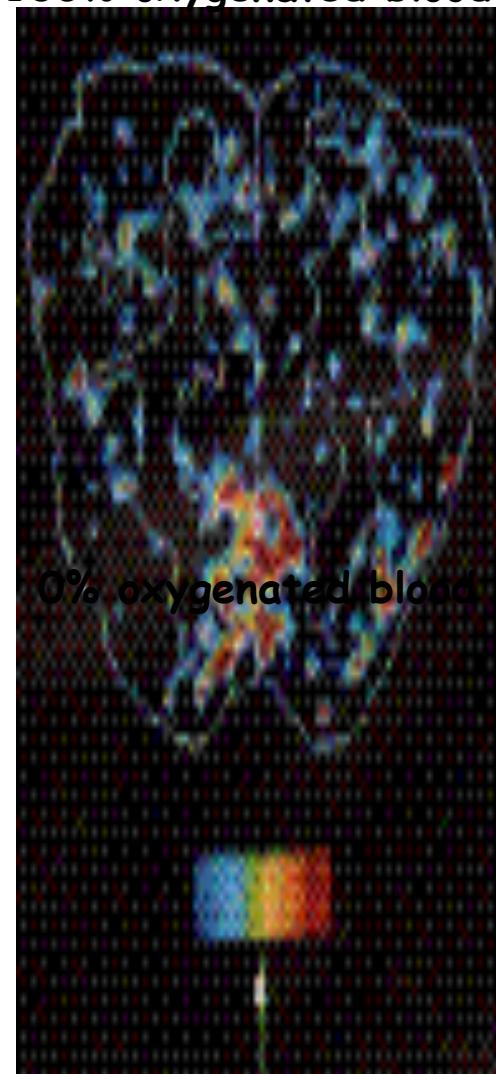
in vivo

$100\% O_2$



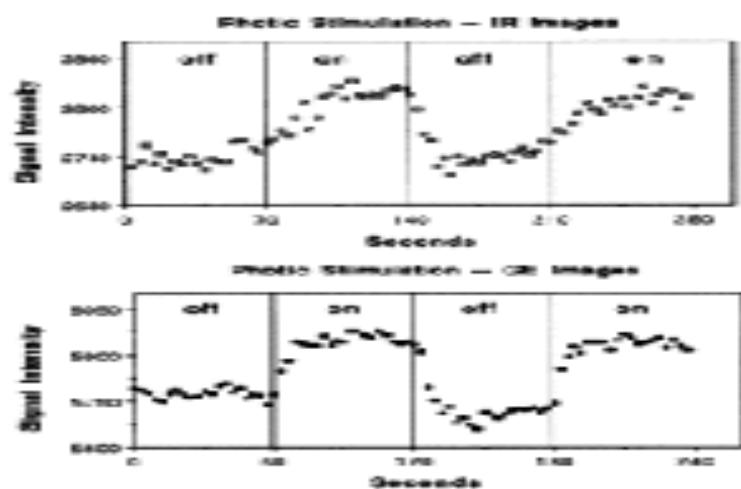
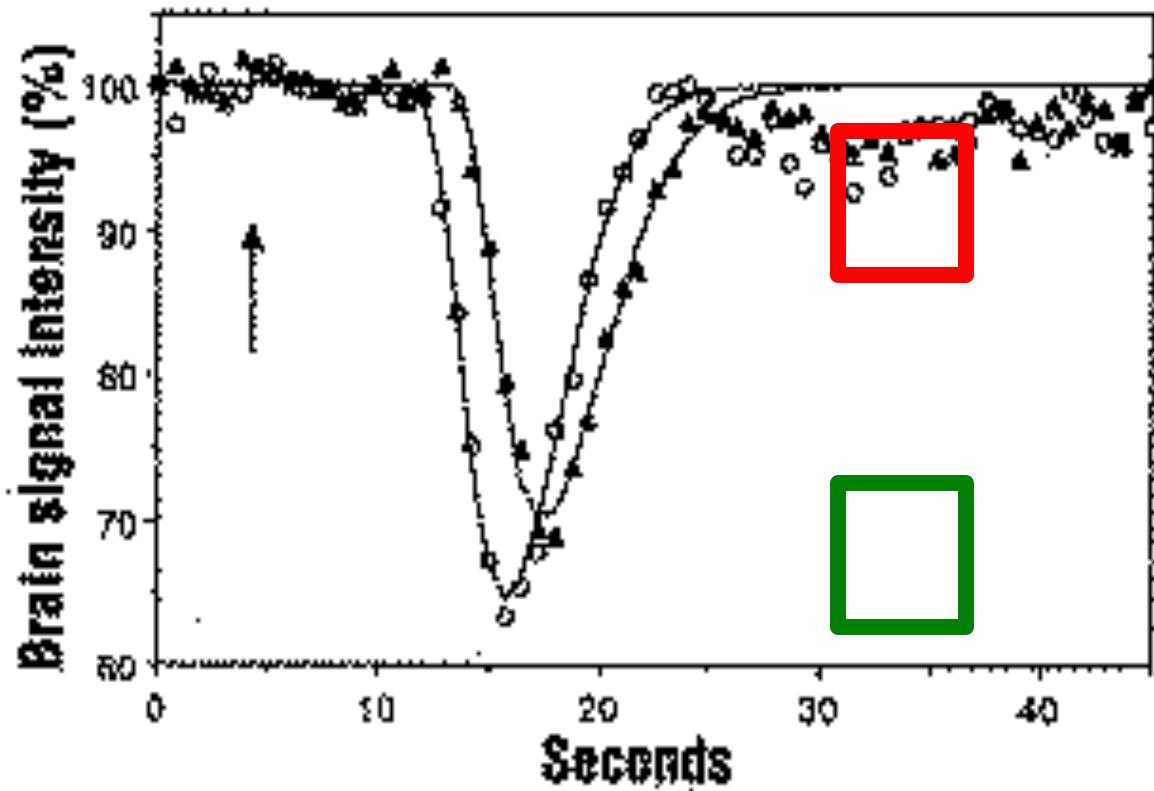
in vitro

$100\% \text{ oxygenated blood}$



$20\% O_2$

S. Ogawa, T.-M. Lee, A. S. Nayak, P. Glynn, Magn. Reson. Med., 14, 68-78 (1990)



R. Turner, D. LeBihan, C.T.W. Moonen, D. Despres, J. Frank, Magn. Reson. Med., 22, 159-166 (1991)

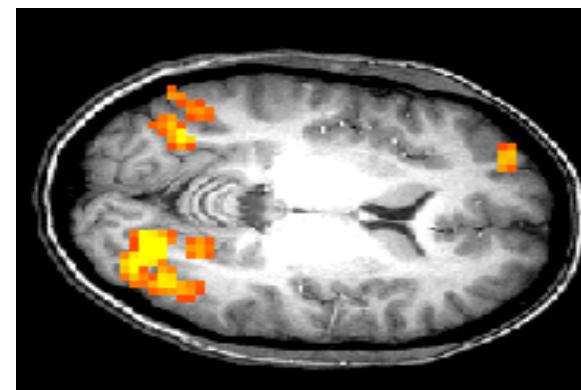
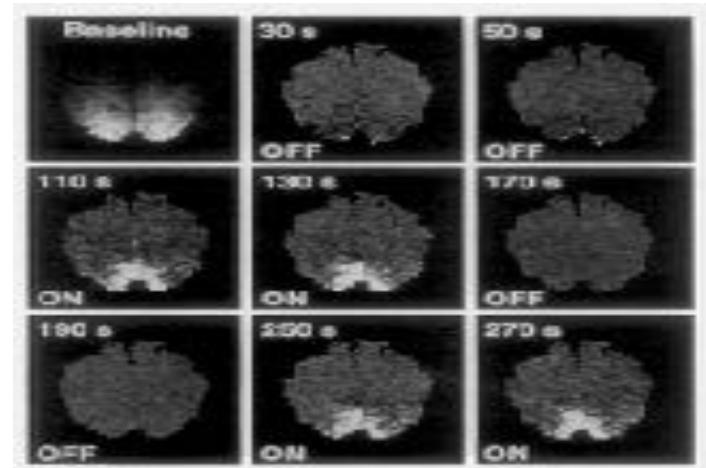
**1. A bit of history of MRI
and functional MRI**

**2. Basics of functional MRI
contrast and methods**

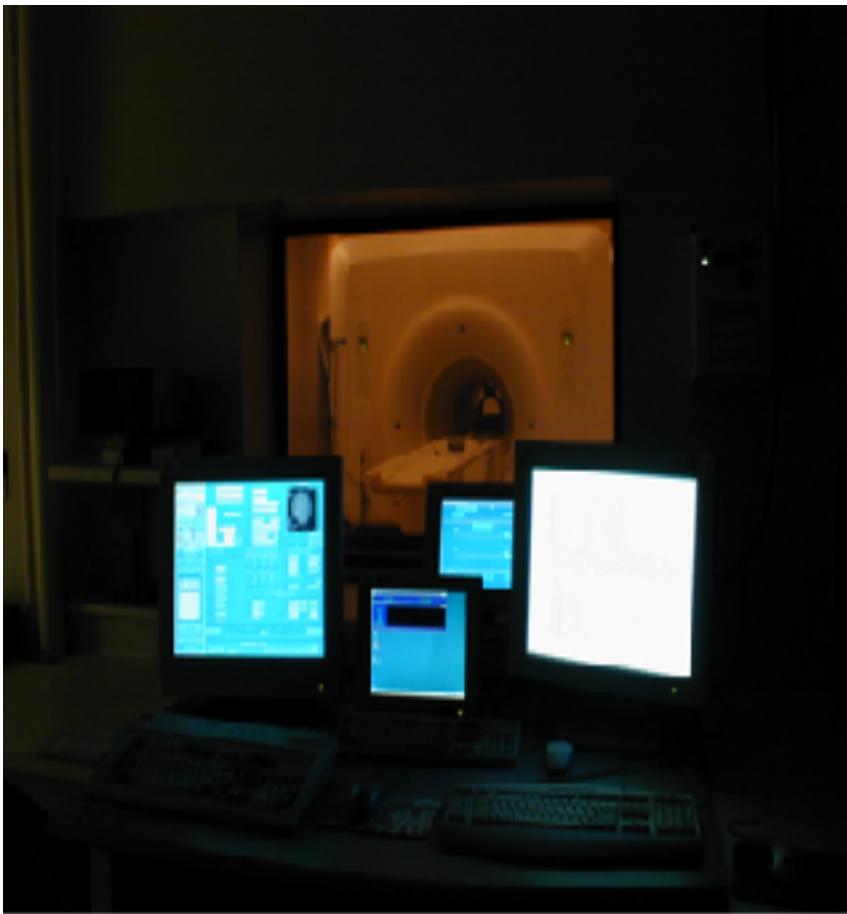
**3. Basic and cutting edge
applications**

Blood Volume Imaging

Susceptibility Contrast agent bolus injection and time series collection of T2* or T2 - weighted images

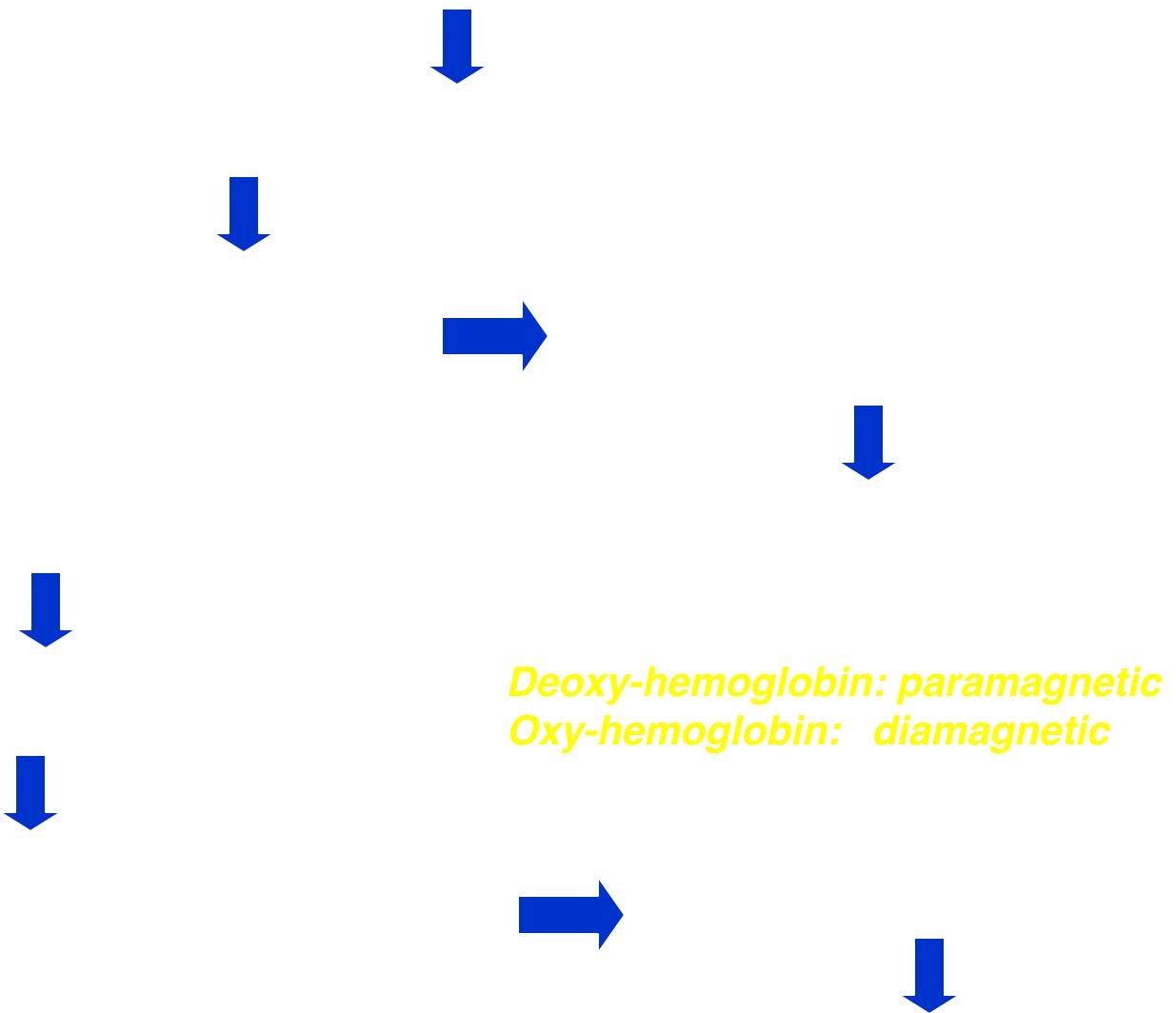


Kwong et al.

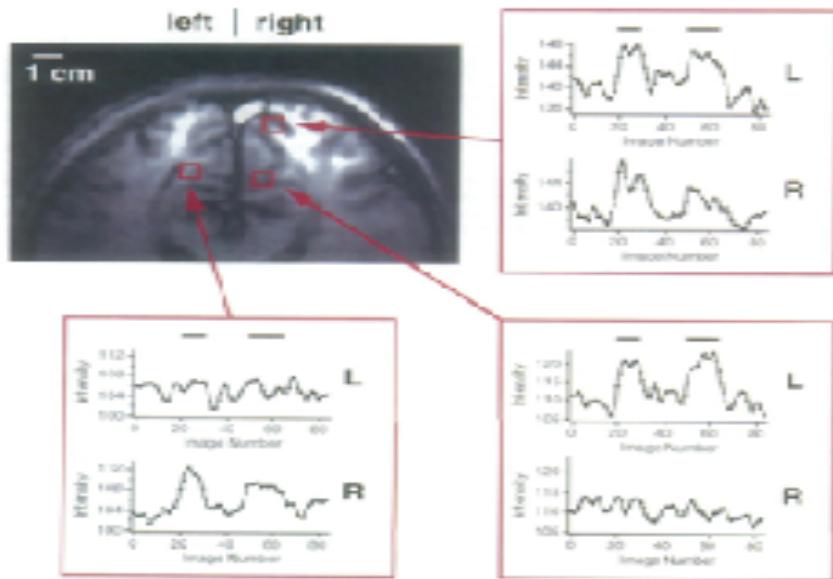


K. K. Kwong, et al, (1992) "Dynamic magnetic resonance imaging of human brain activity during primary sensory stimulation." Proc. Natl. Acad. Sci. USA. 89, 5675-5679.

BOLD Contrast in the Detection of Neuronal Activity



Ogawa et al.



S. Ogawa, et al., (1992) "Intrinsic signal changes accompanying sensory stimulation: functional brain mapping with magnetic resonance imaging. Proc. Natl. Acad. Sci. USA." 89, 5951-5955.

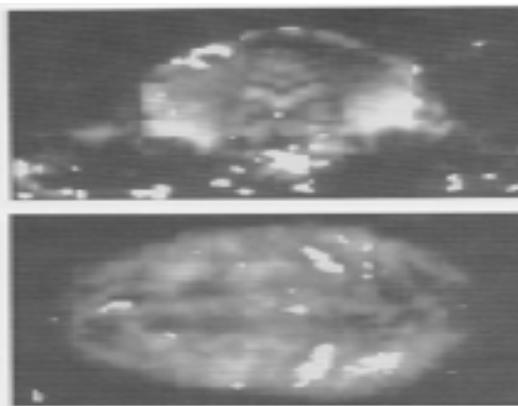
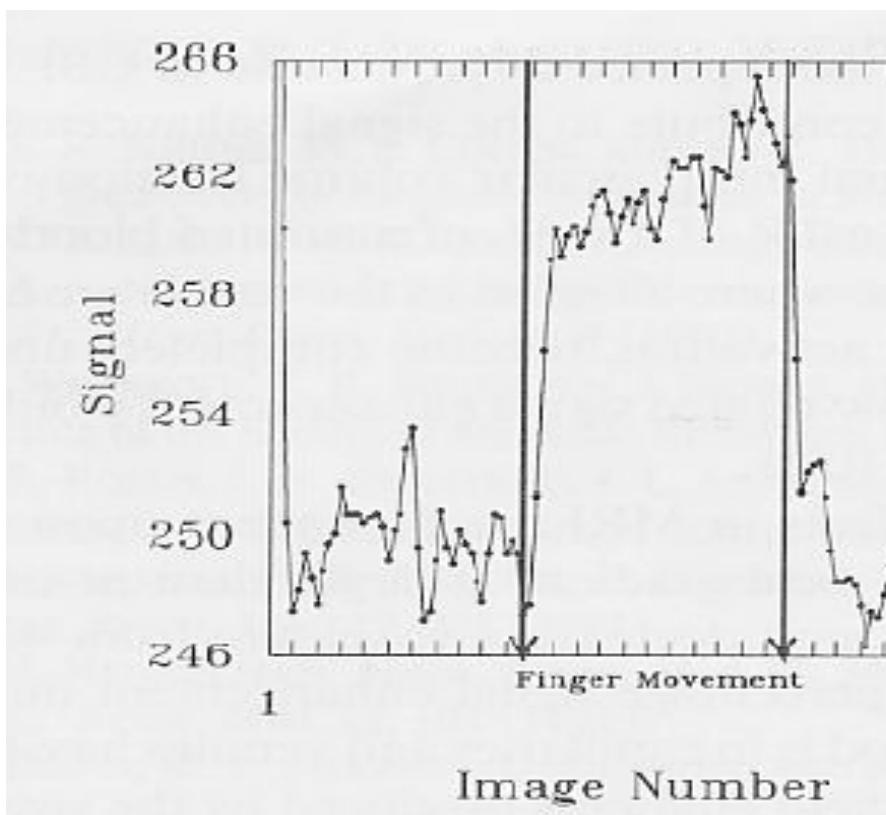
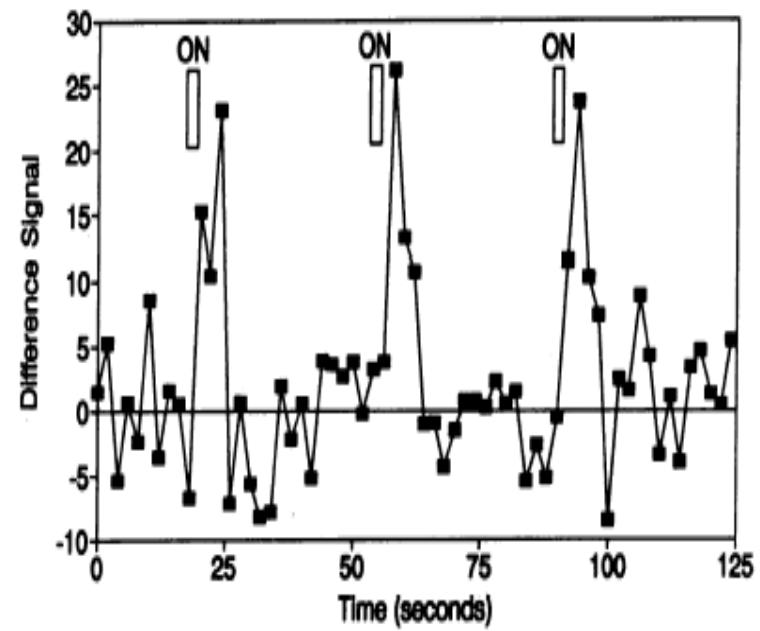
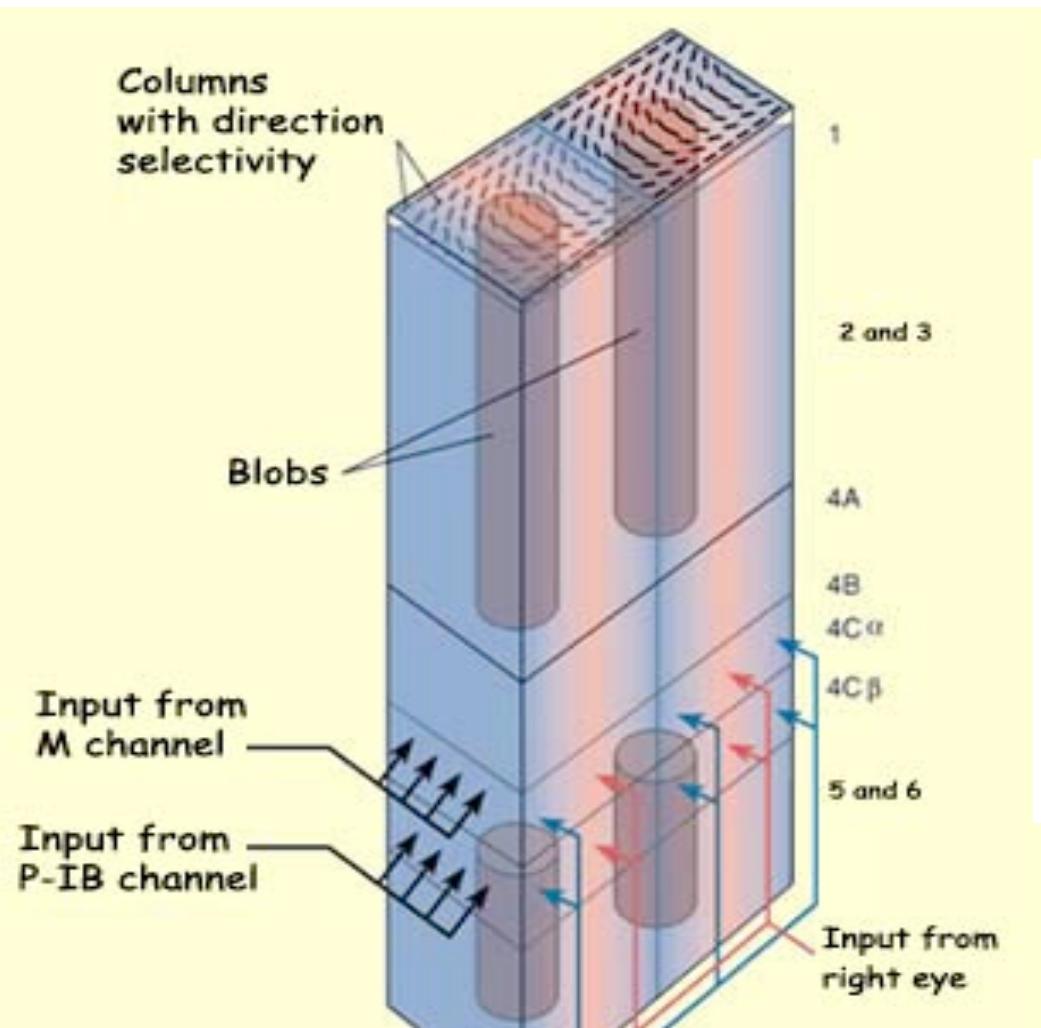


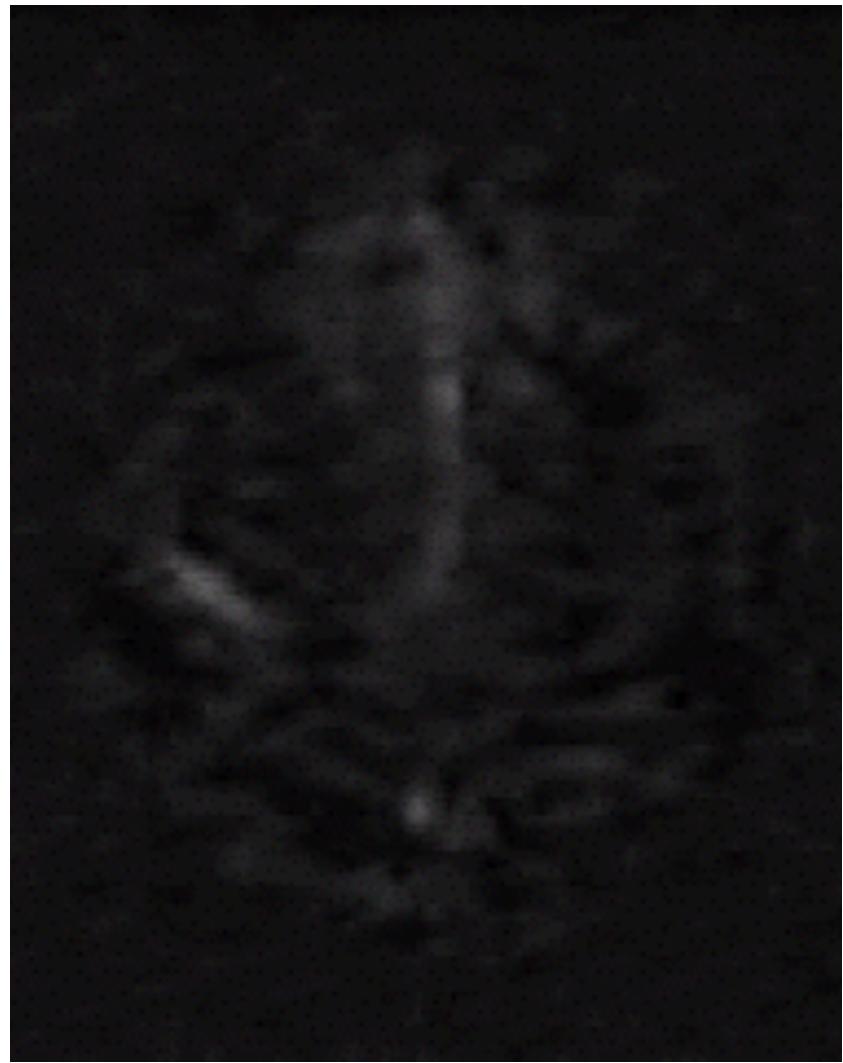
Fig. 2. Magnetic-resonance-signal changes in fMRI images. (Top) Slices at 200 mm, anterior-posterior (AP)-posterior commissure (PC)-anterior commissure (AC) plane; (bottom) slices at 200 mm, anterior (A)-posterior (P)-left lateral (LL)-right lateral (RL) plane. (Left) Corresponding blood-flow images (per image frame). (Right) Corresponding fMRI images. (a) Unthresholded fMRI images. (b) fMRI images thresholded at $P < 0.05$.



Bandettini et al.



P. A. Bandettini, et al., (1992) "Time course EPI of human brain function during task activation." Magn. Reson. Med 25, 390-397.



1991

Blamire et al.



• Blamire, A. M., et al. (1992). "Dynamic mapping of the human visual cortex by high-speed magnetic resonance imaging." *Proc. Natl. Acad. Sci. USA* 89: 11069-11073.

1992...Perfusion using Arterial Spin Labeling

Williams, D. S., Detre, J. A., Leigh, J. S. & Koretsky, A. S. (1992) "Magnetic resonance imaging of perfusion using spin-inversion of arterial water." *Proc. Natl. Acad. Sci. USA* **89**, 212-216.

Edelman, R., Siewert, B. & Darby, D. (1994) "Qualitative mapping of cerebral blood flow and functional localization with echo planar MR imaging and signal targeting with alternating radiofrequency (EPISTAR)." *Radiology* **192**, 1-8.

Kim, S.-G. (1995) "Quantification of relative cerebral blood flow change by flow-sensitive alternating inversion recovery (FAIR) technique: application to functional mapping." *Magn. Reson. Med.* **34**, 293-301.

Kwong, K. K. et al. (1995) "MR perfusion studies with T1-weighted echo planar imaging." *Magn. Reson. Med.* **34**, 878-887.

Contrast in Functional MRI

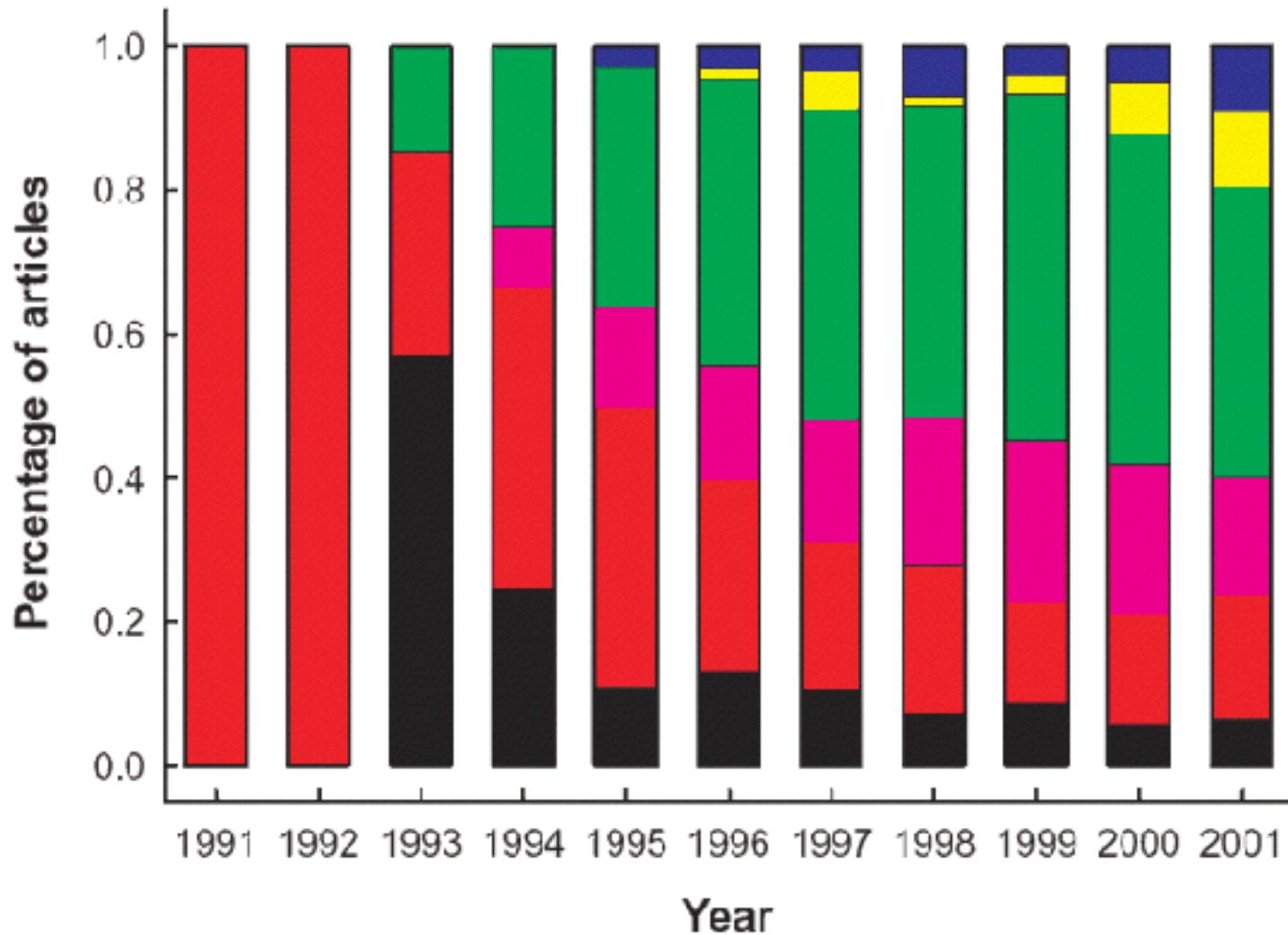
- Blood Volume
- Blood Oxygenation Changes
- Blood Perfusion

fMRI Contrast

- Volume (gadolinium)
- BOLD
- Perfusion (ASL)
- ΔCMRO_2
- Δ Volume (VASO)
- Neuronal Currents
- Diffusion coefficient
- Temperature

Scopus: Articles or Reviews Published per Year

“fMRI” or “functional MRI”



Motor (black)
Primary Sensory (red)
Integrative Sensory (violet)
Basic Cognition (green)
High-Order Cognition (yellow)
Emotion (blue)

J. Illes, M. P. Kirschen, J. D. E. Gabrielli, Nature Neuroscience, 6 (3)m p.205

Log Size (mm)

Brain

Map

Column

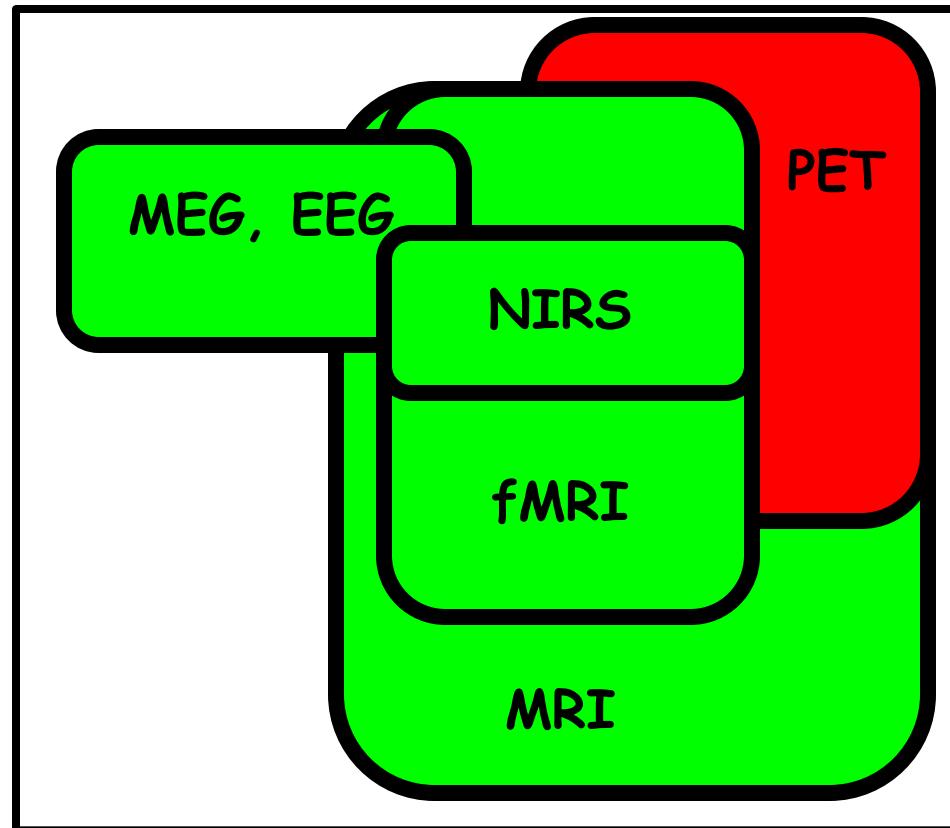
Layer

3
2
1
0
-1

-3 -2 -1 0 1 2 3 4 5 6 7

Millisecond Second Minute Hour Day

Log Time (sec)

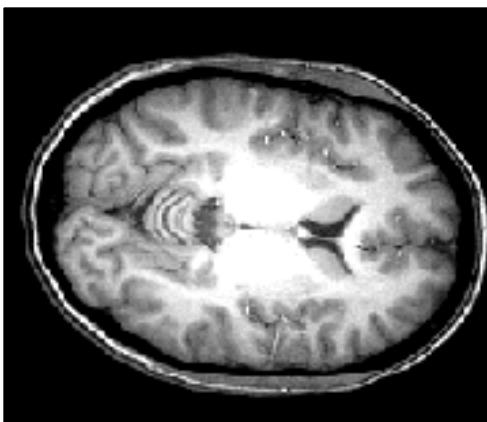


Topics Studied with fMRI at the NIH

- Epilepsy
- Visual processing
- Mood disorders
- Learning
- Habituation
- Plasticity
- Motor Function
- Auditory processing
- Attention
- Language
- Speech
- Stroke
- Social Interaction
- Development
- Aging

MRI vs. fMRI

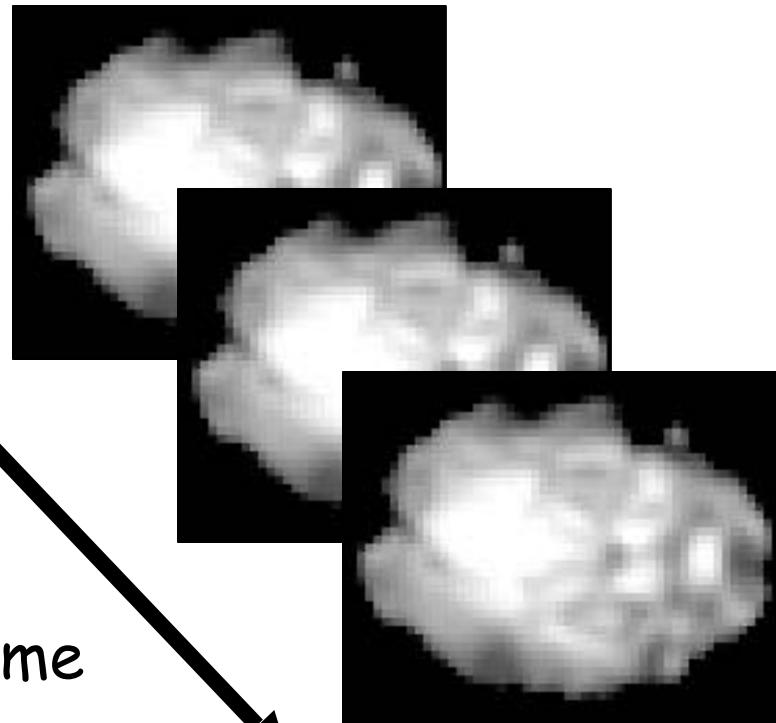
MRI



one image

high resolution
(1 mm or less)

fMRI

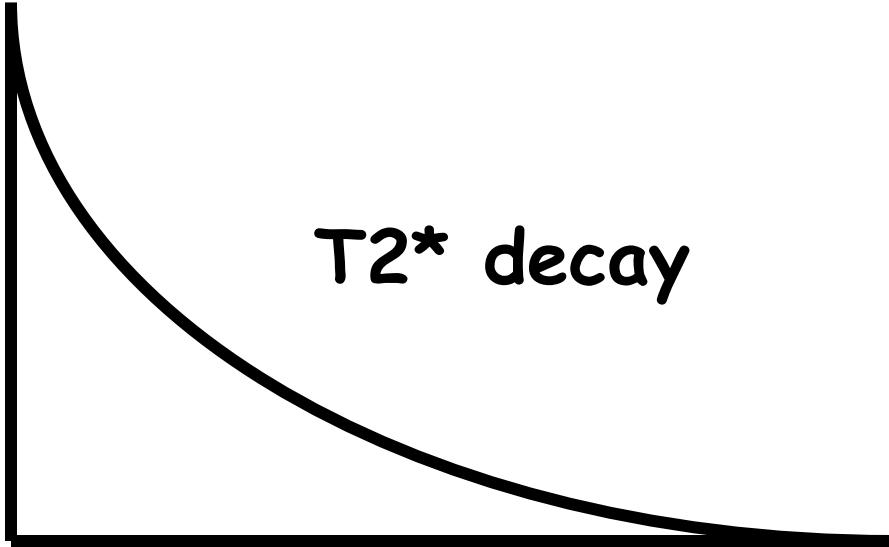


many images

(e.g., every 2 sec for 5 mins)

low resolution
(1.5 to 4 mm)

Single Shot Echo Planar Imaging (EPI)

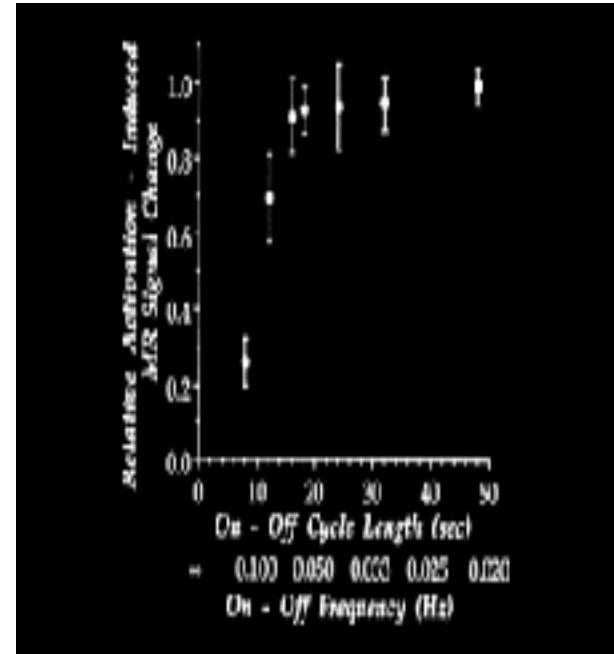


T_{2^*} decay



EPI Readout Window

\approx 20 to 40 ms

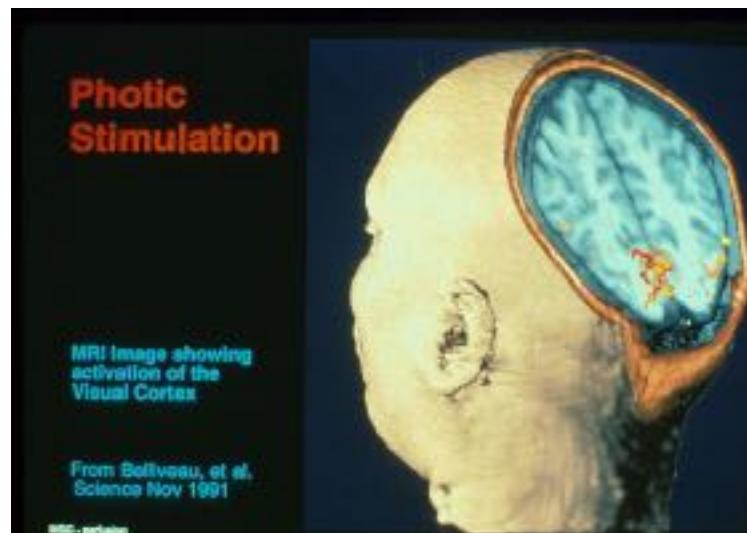




August, 1991

1991-1992

1992-1999



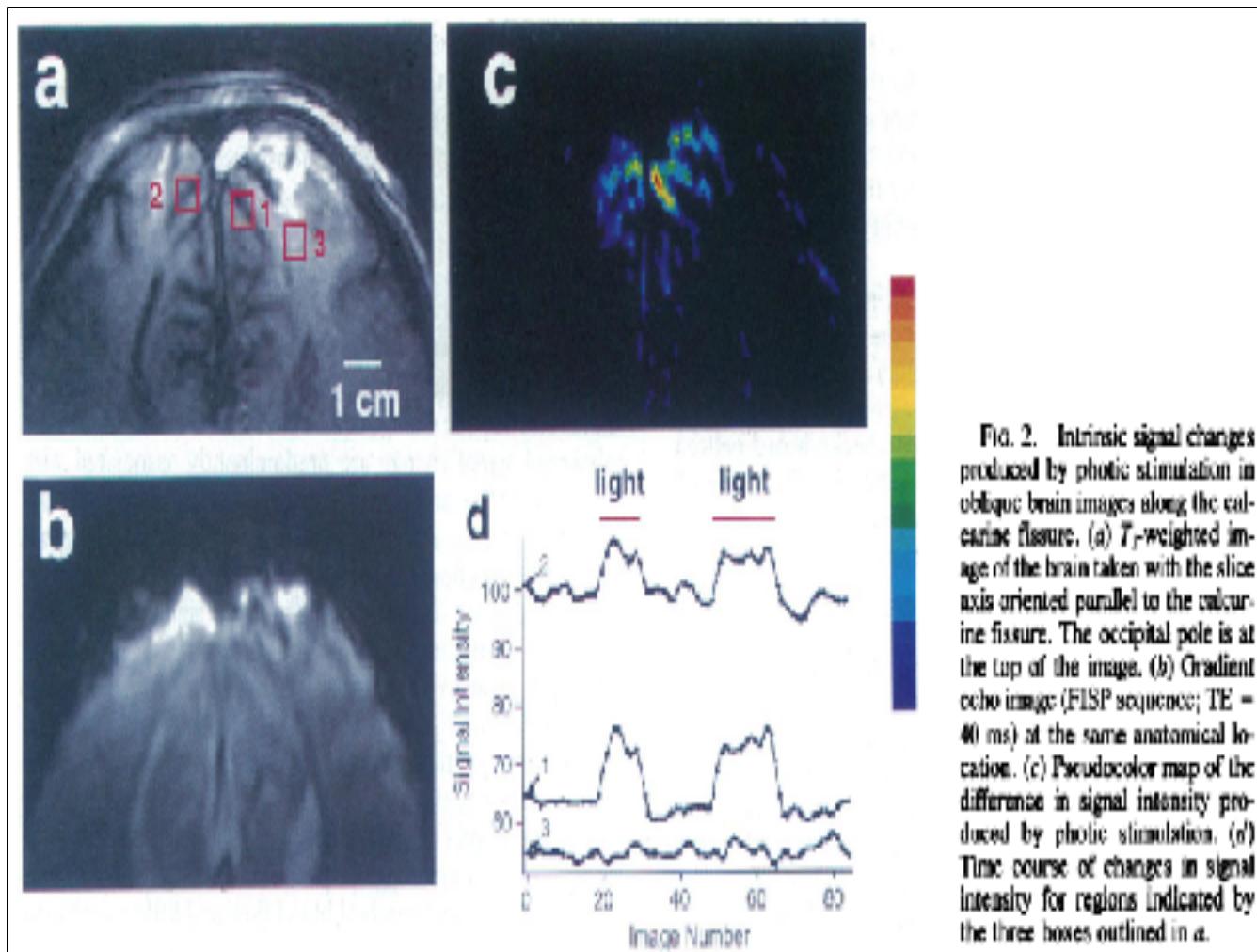
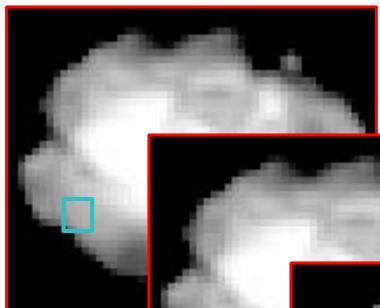


FIG. 2. Intrinsic signal changes produced by photic stimulation in oblique brain images along the calcarine fissure. (a) T_1 -weighted image of the brain taken with the slice axis oriented parallel to the calcarine fissure. The occipital pole is at the top of the image. (b) Gradient echo image (FISP sequence; TE = 40 ms) at the same anatomical location. (c) Pseudocolor map of the difference in signal intensity produced by photic stimulation. (d) Time course of changes in signal intensity for regions indicated by the three boxes outlined in a.

Activation Statistics

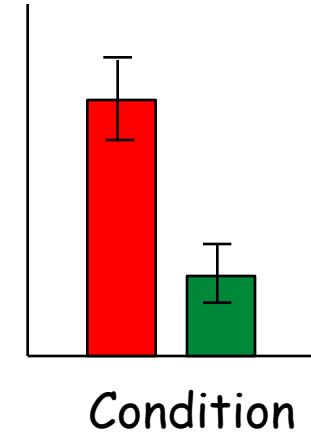
Functional images



~2s

fMRI
Signal
(% change)

ROI
Time
Course



Condition

Condition 1

Time

Condition 2

~ 5 min

Region of interest (ROI)

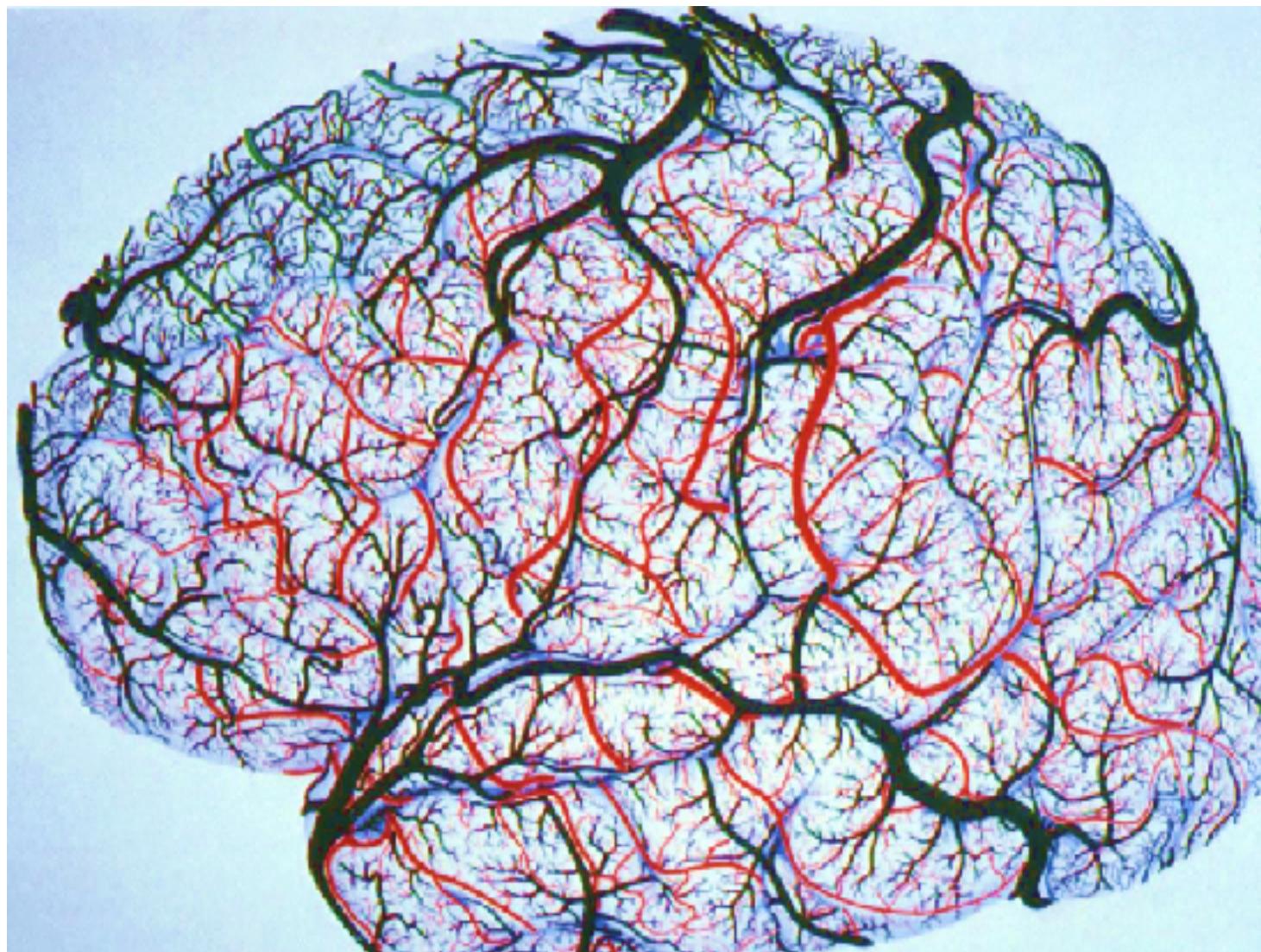
Statistical Map
superimposed on
anatomical MRI image



fMRI Setup



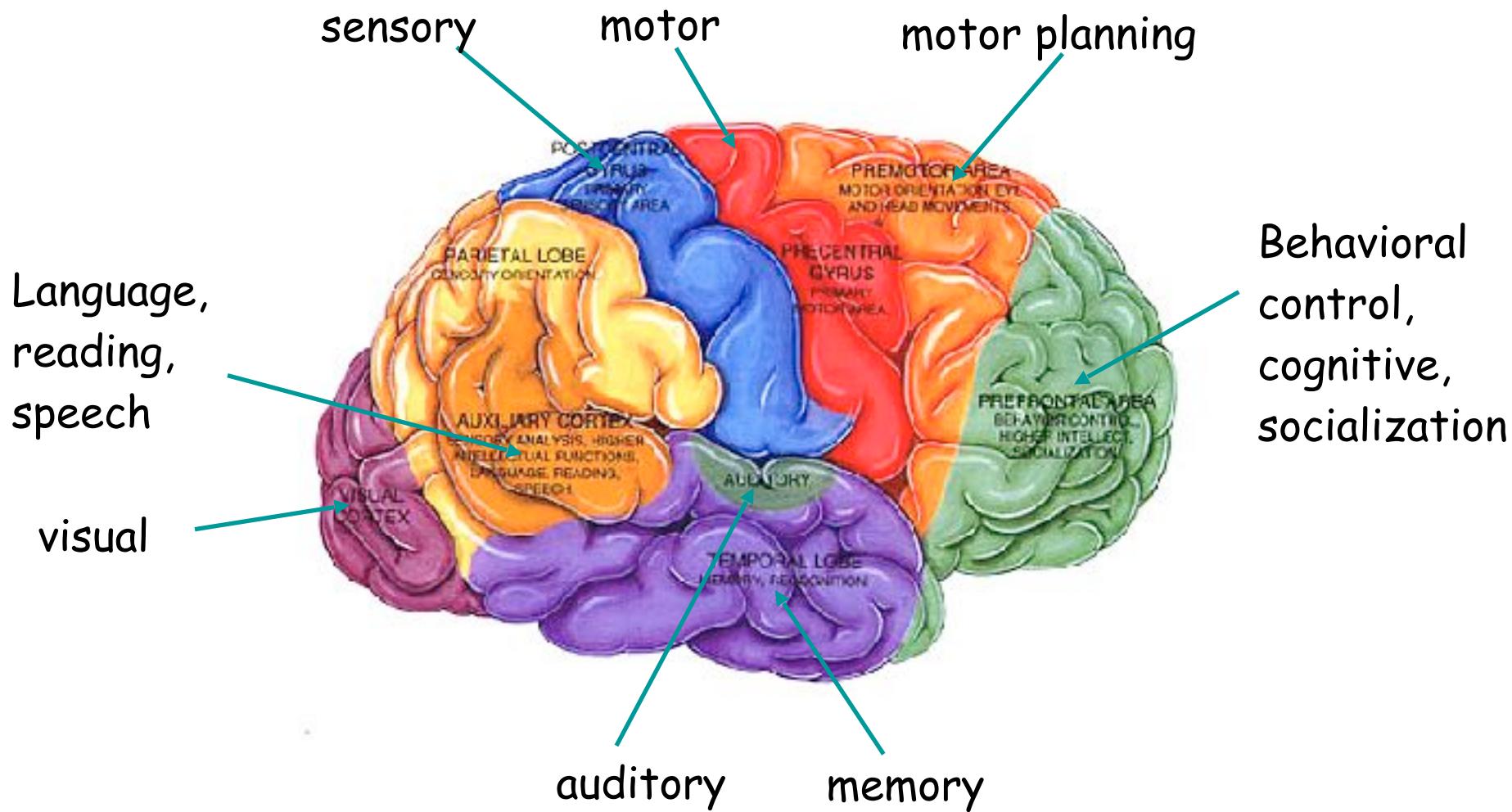
Courtesy, Robert Cox,
Scientific and Statistical
Computing Core Facility,
NIMH

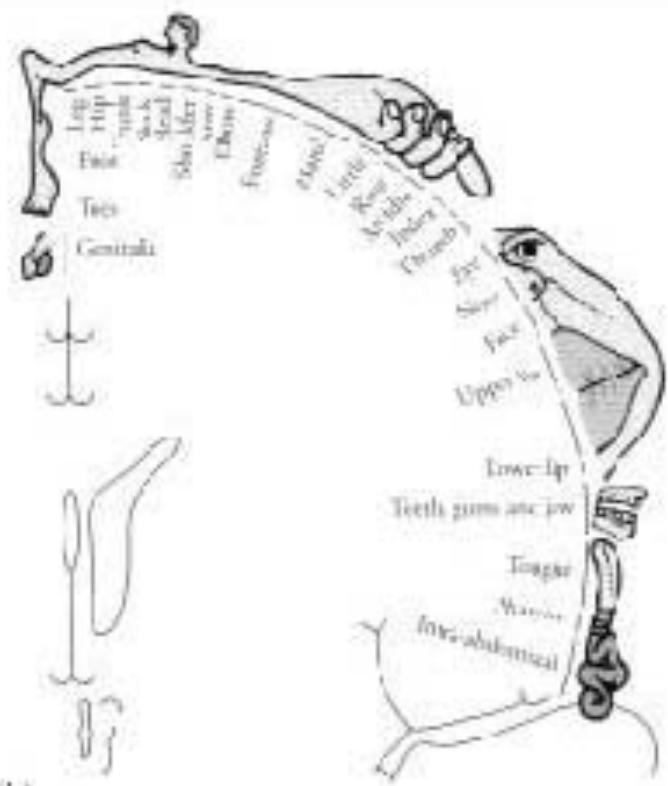
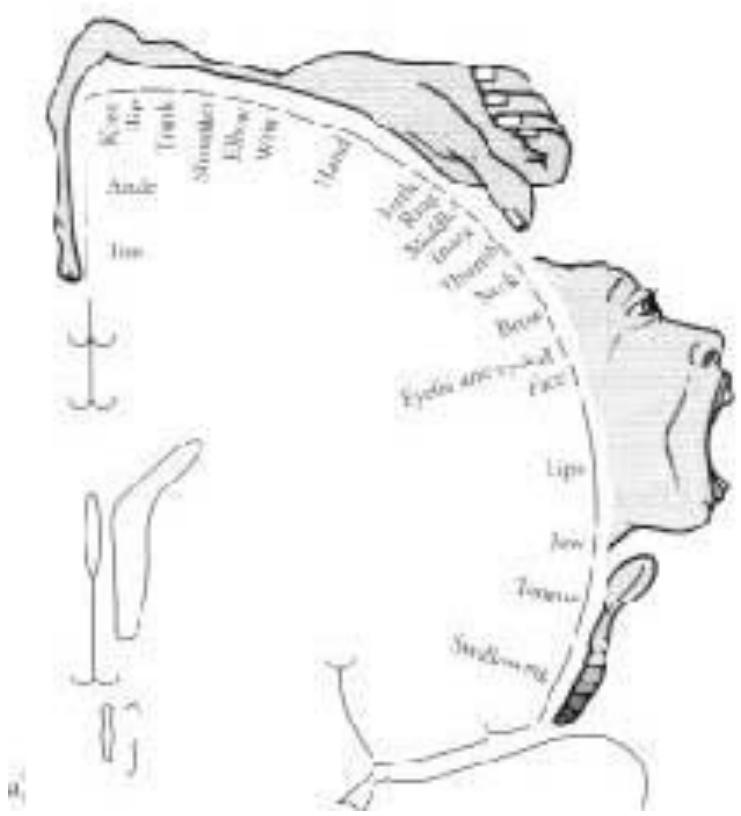


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2. Basics of functional MRI contrast and methods
3. Basic and cutting edge applications

Motor Cortex

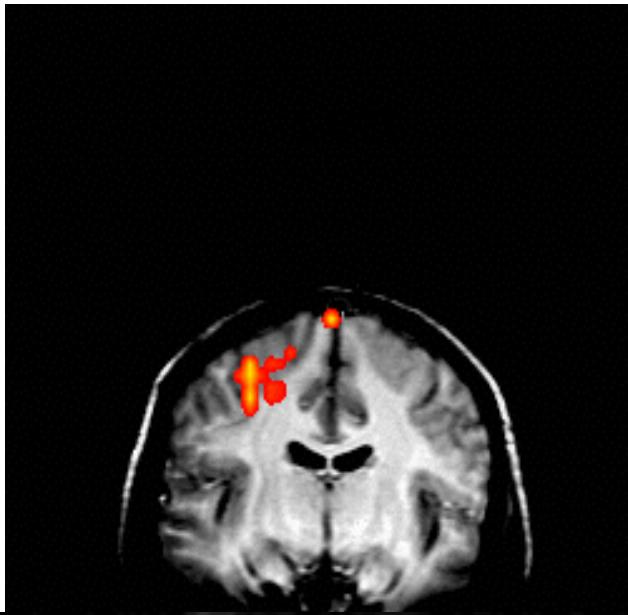
Brain Function



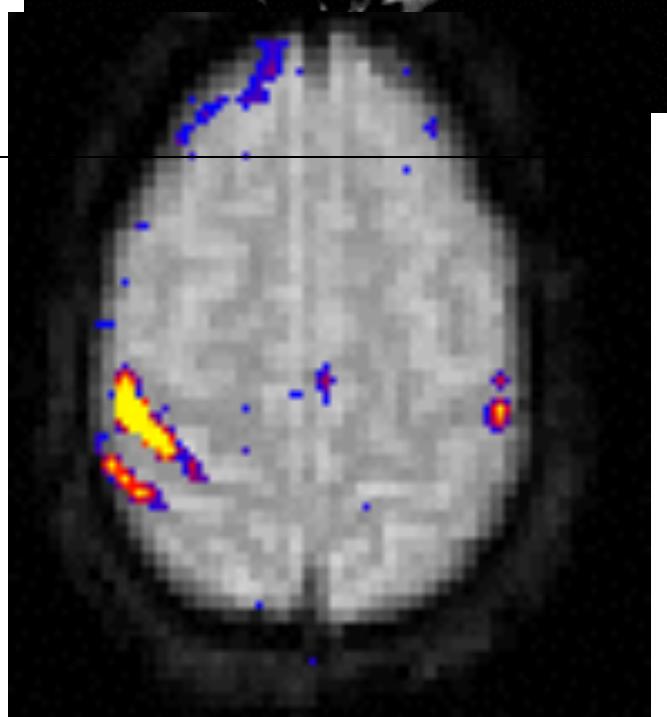
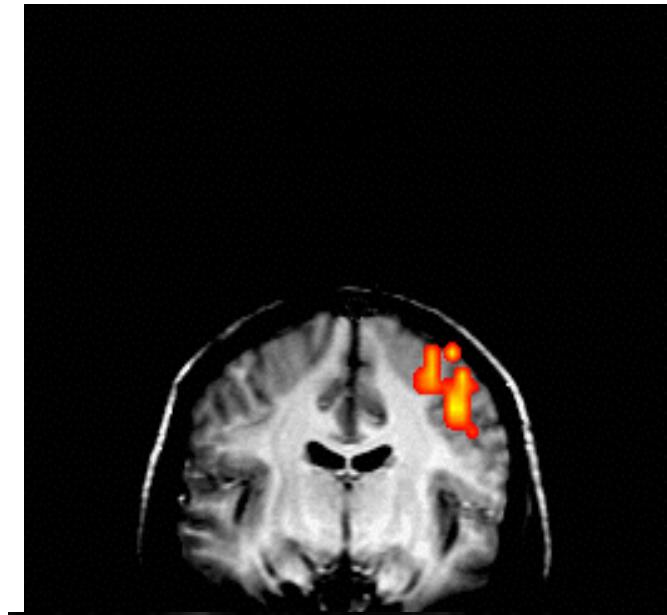
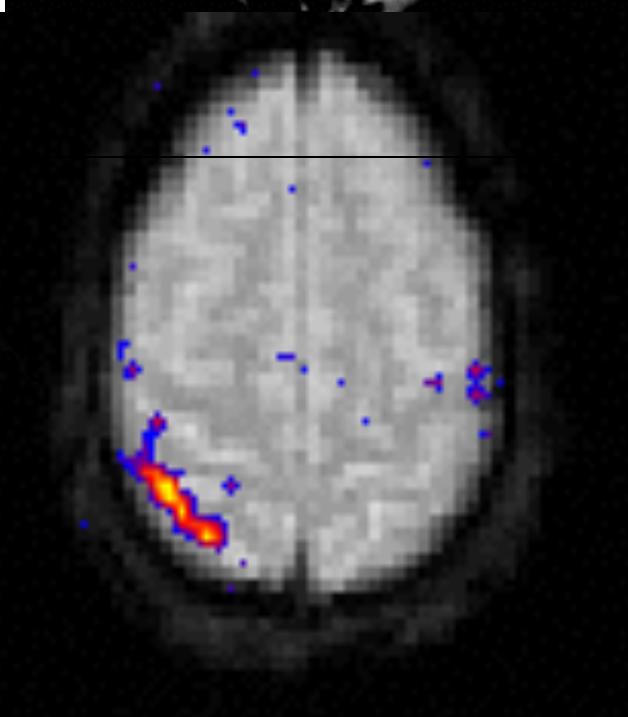


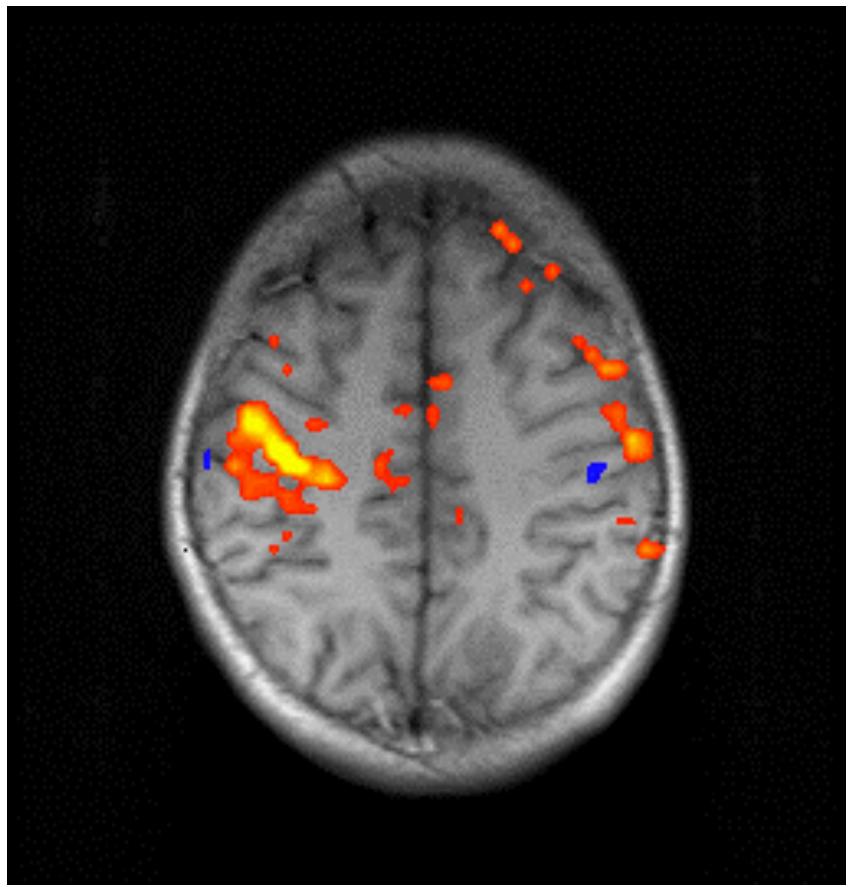
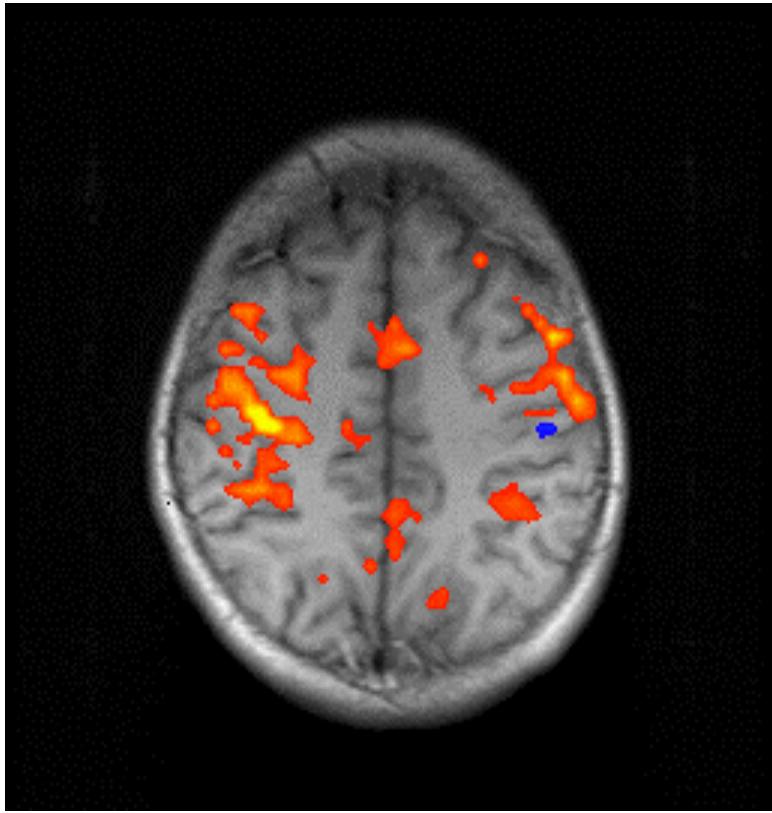
(b)

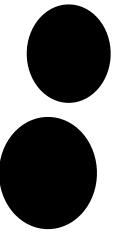
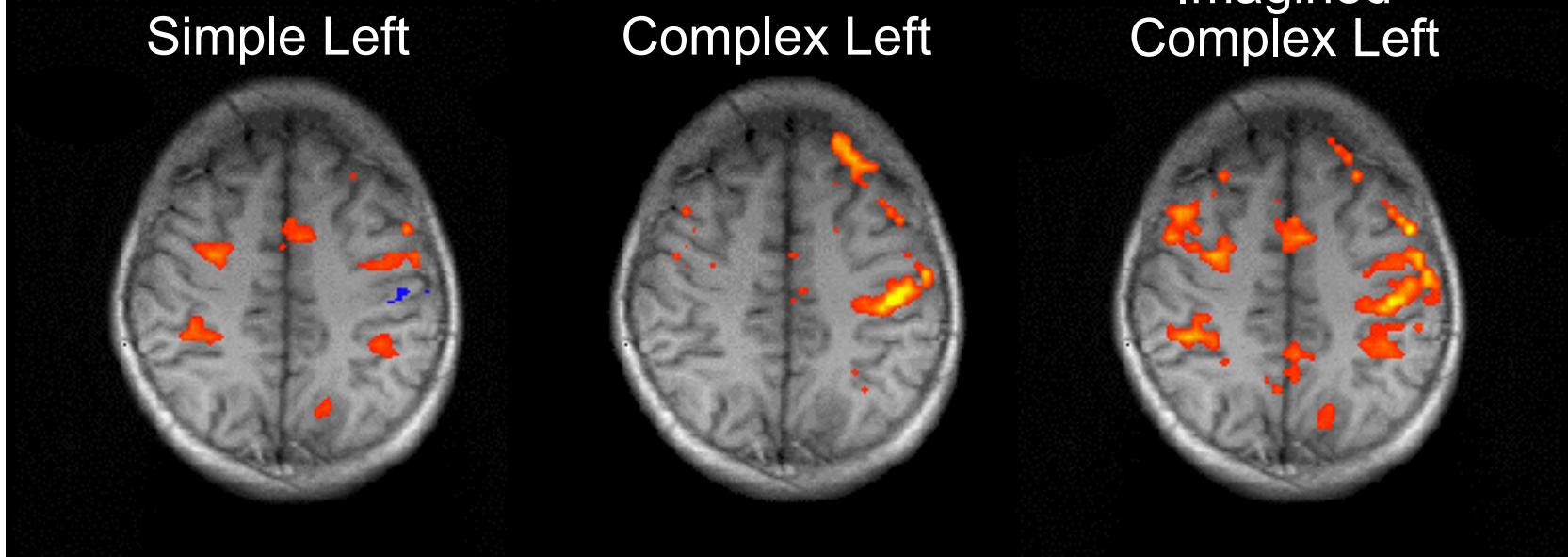
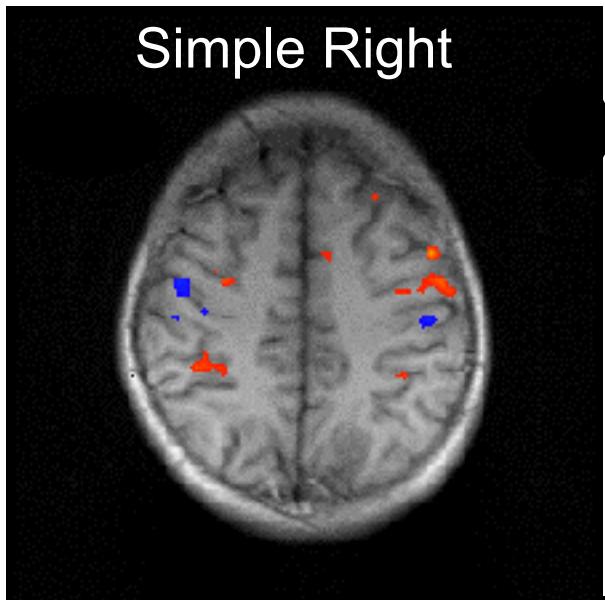
Toe movement



Finger movement







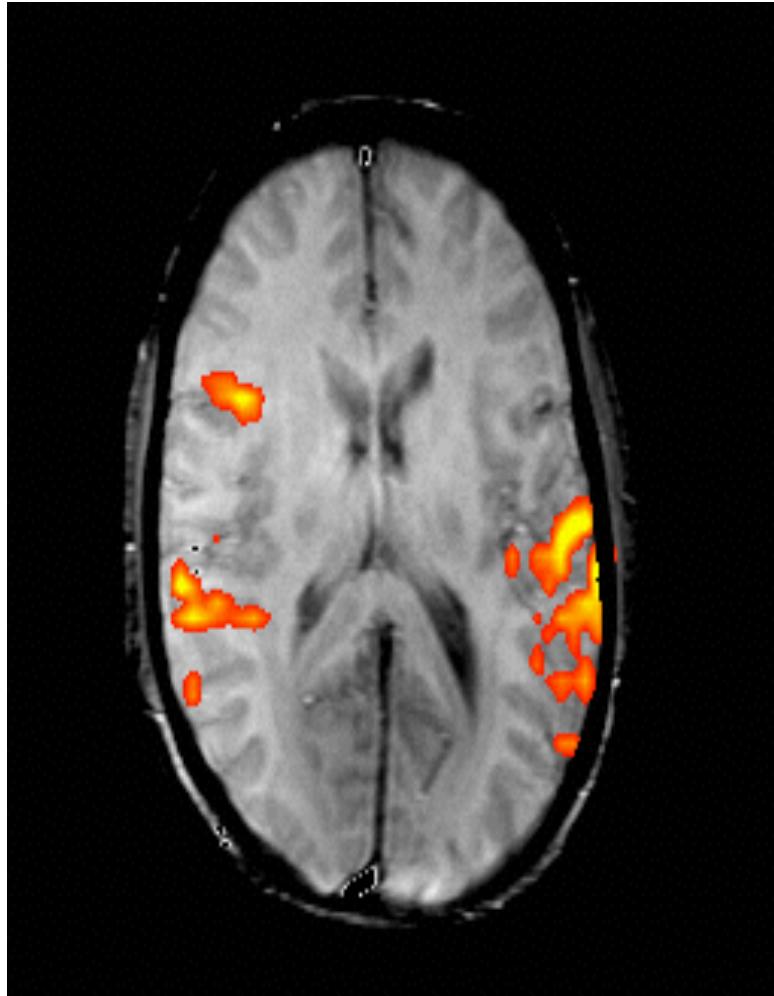
Presurgical Mapping

Left Foot

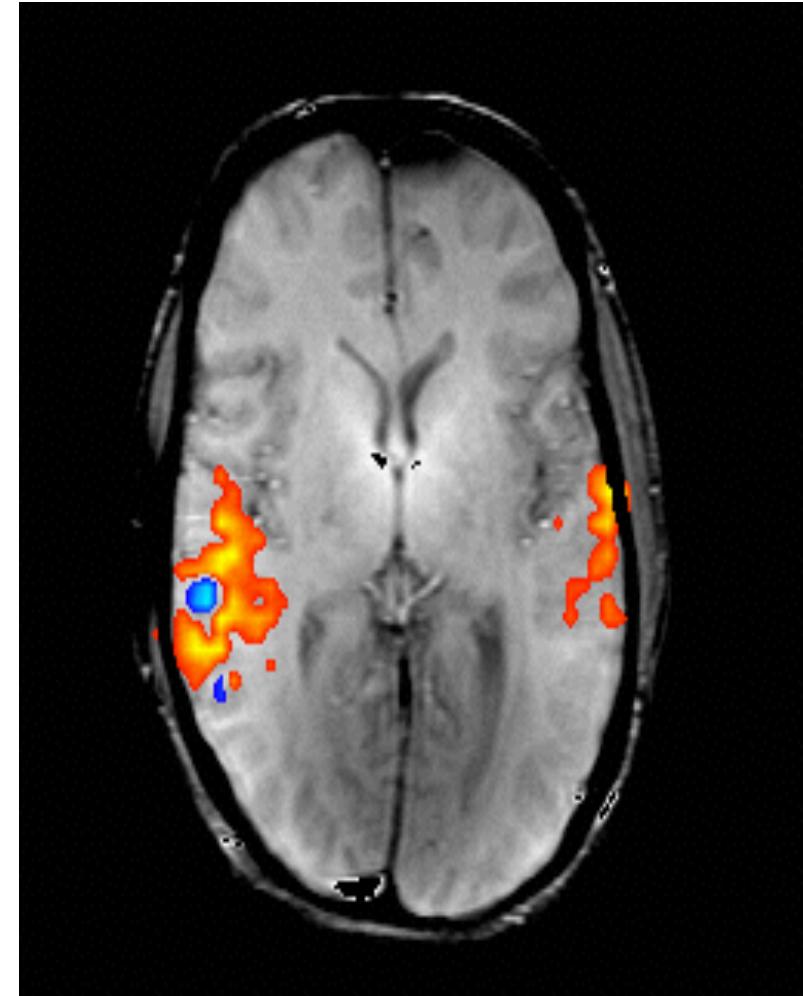
Tumor

Right Foot

Right Hand



fMRI

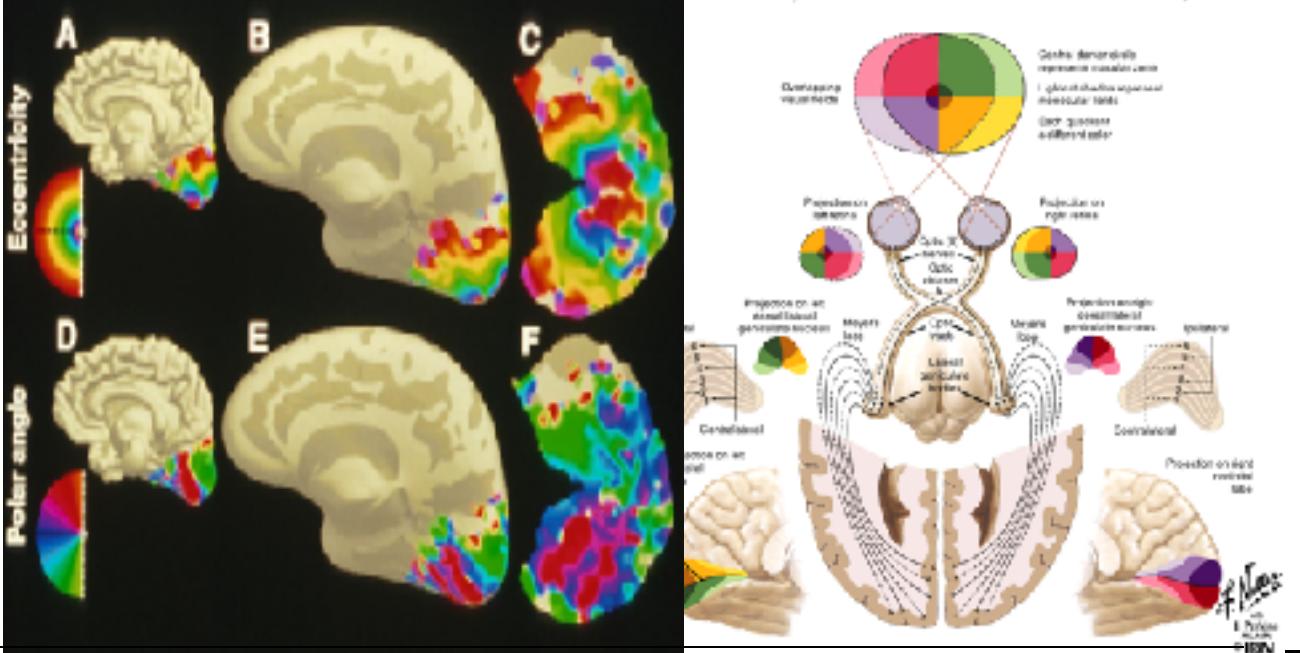


O-15 PET

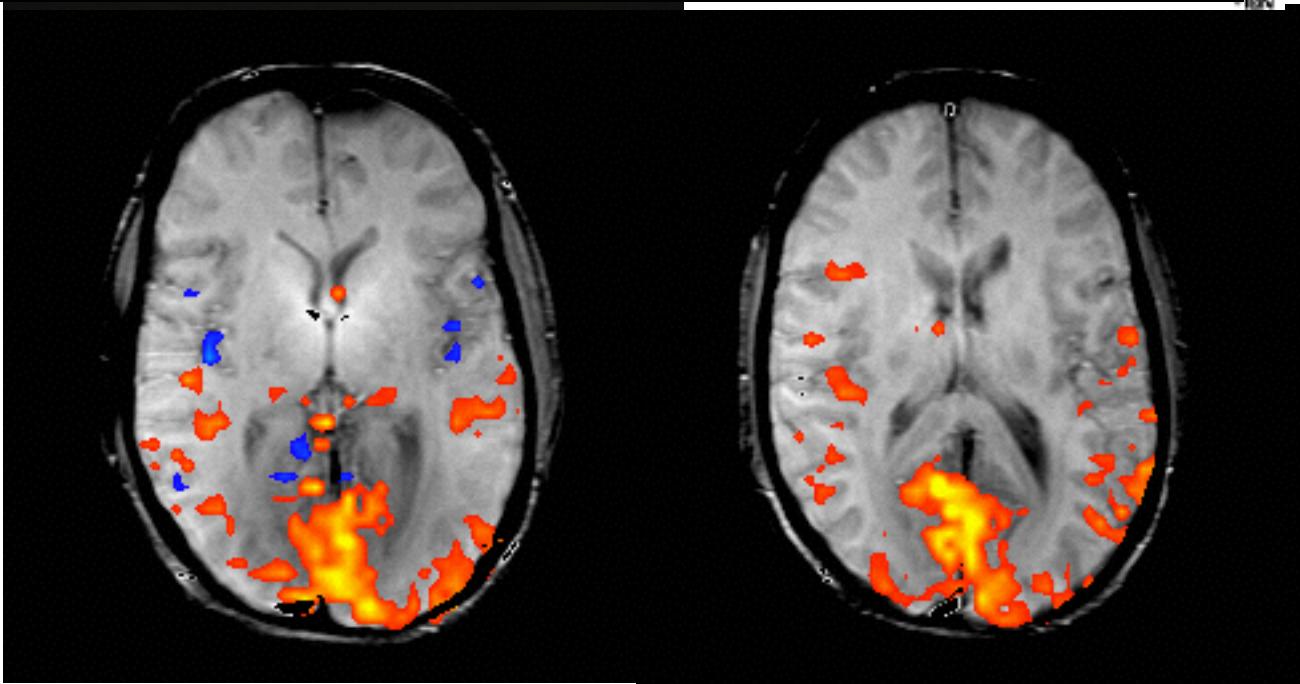
Visual and Auditory Processing

Visual Pathways: The Retino-Geniculo-Calcarine Pathway

Reading

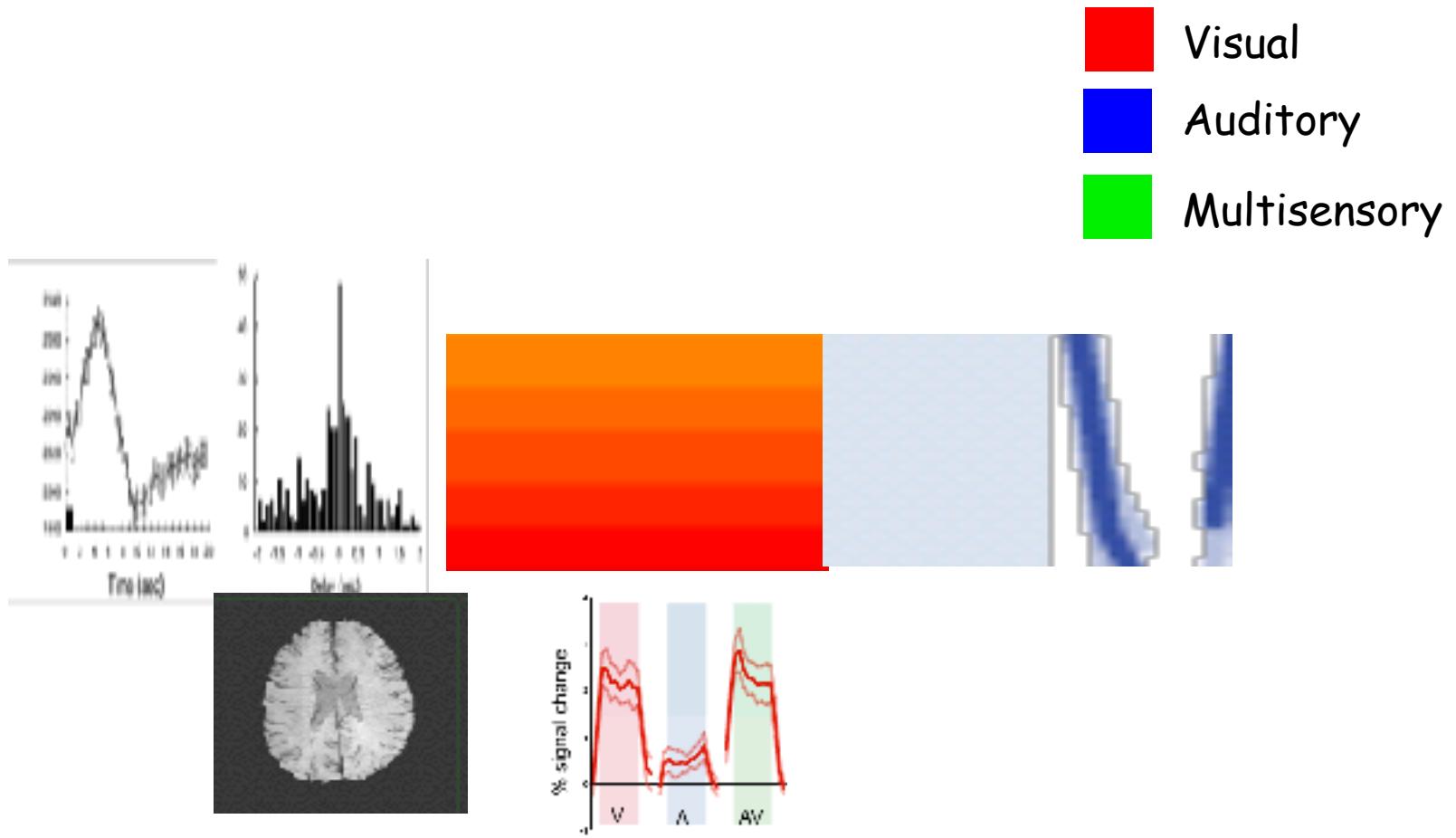


Listening

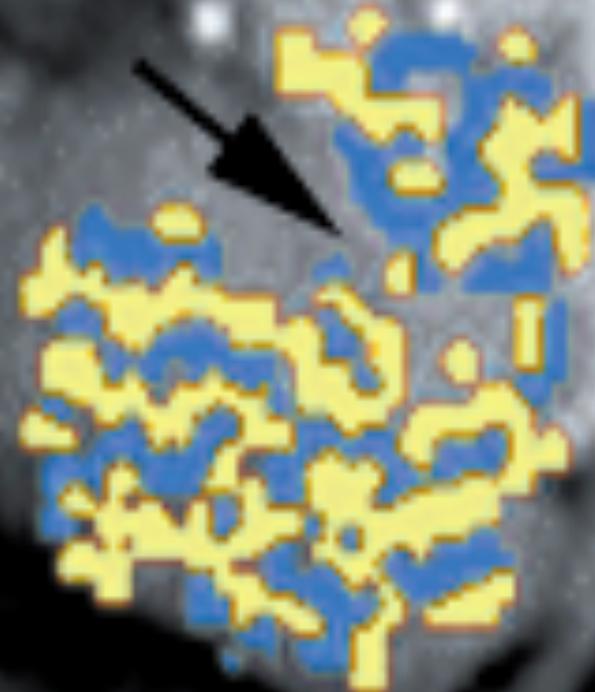


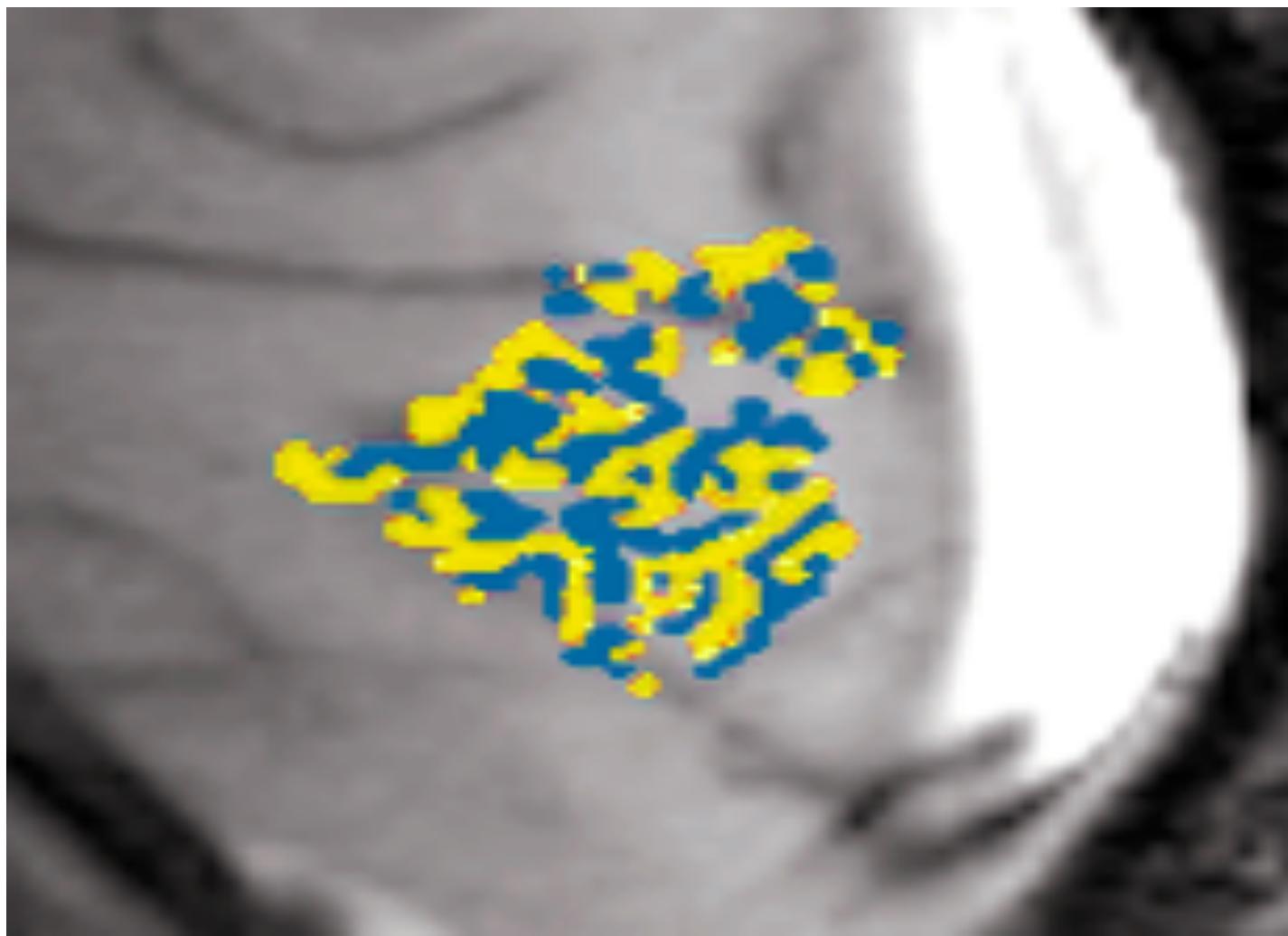
Multi-sensory integration

M.S. Beauchamp et al.,



1 cm

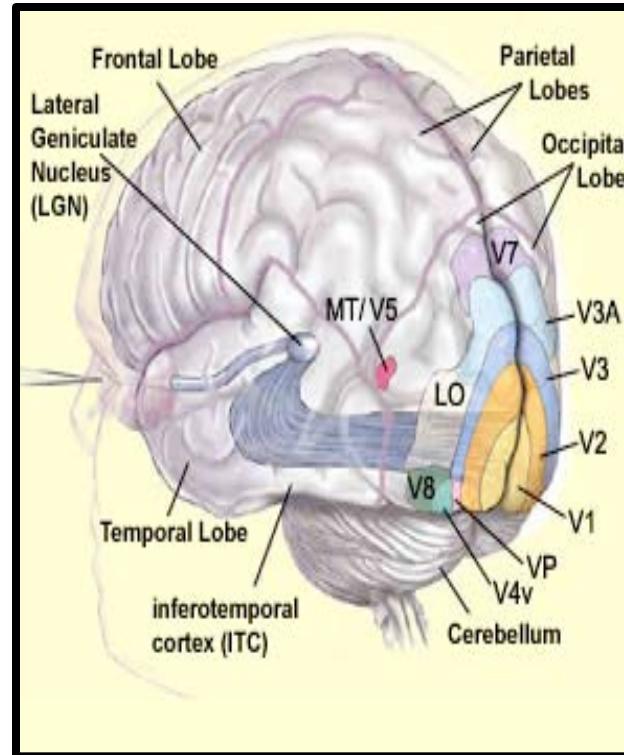
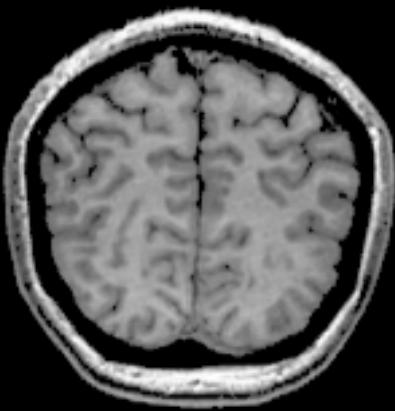




Visual Processing

(spatial resolution)

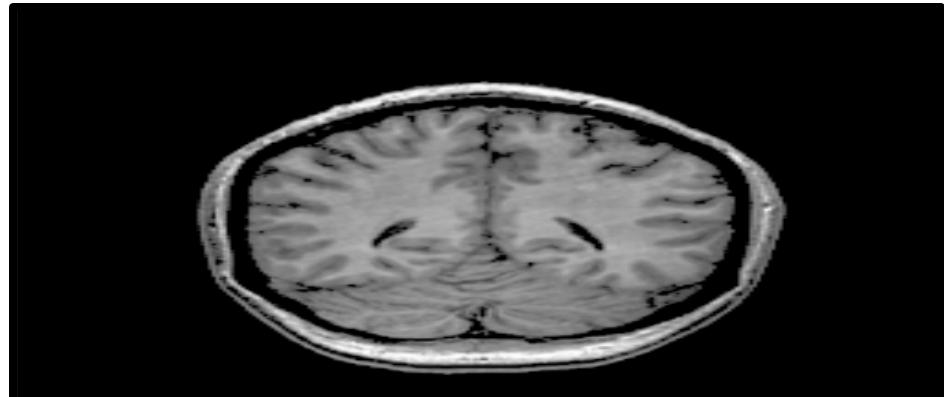
Visual Cortex Organization



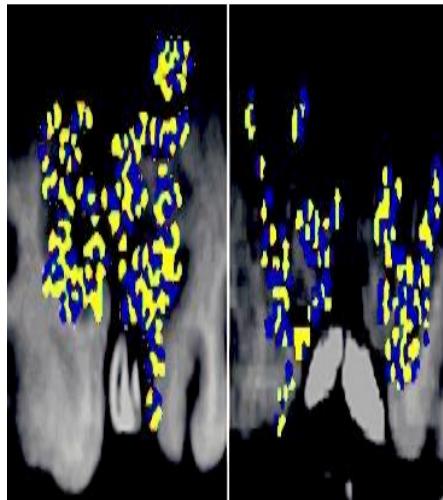
Functional Magnetic Resonance Imaging in Medicine and Physiology

CHRIT T. W. MOONEN, PETER C. M. VAN ZIJL, JOSEPH A. FRANK,
DENIS LE BIHAN, EDWIN D. BECKER

<http://www.thebrain.mcgill.ca>



ODC Maps using fMRI

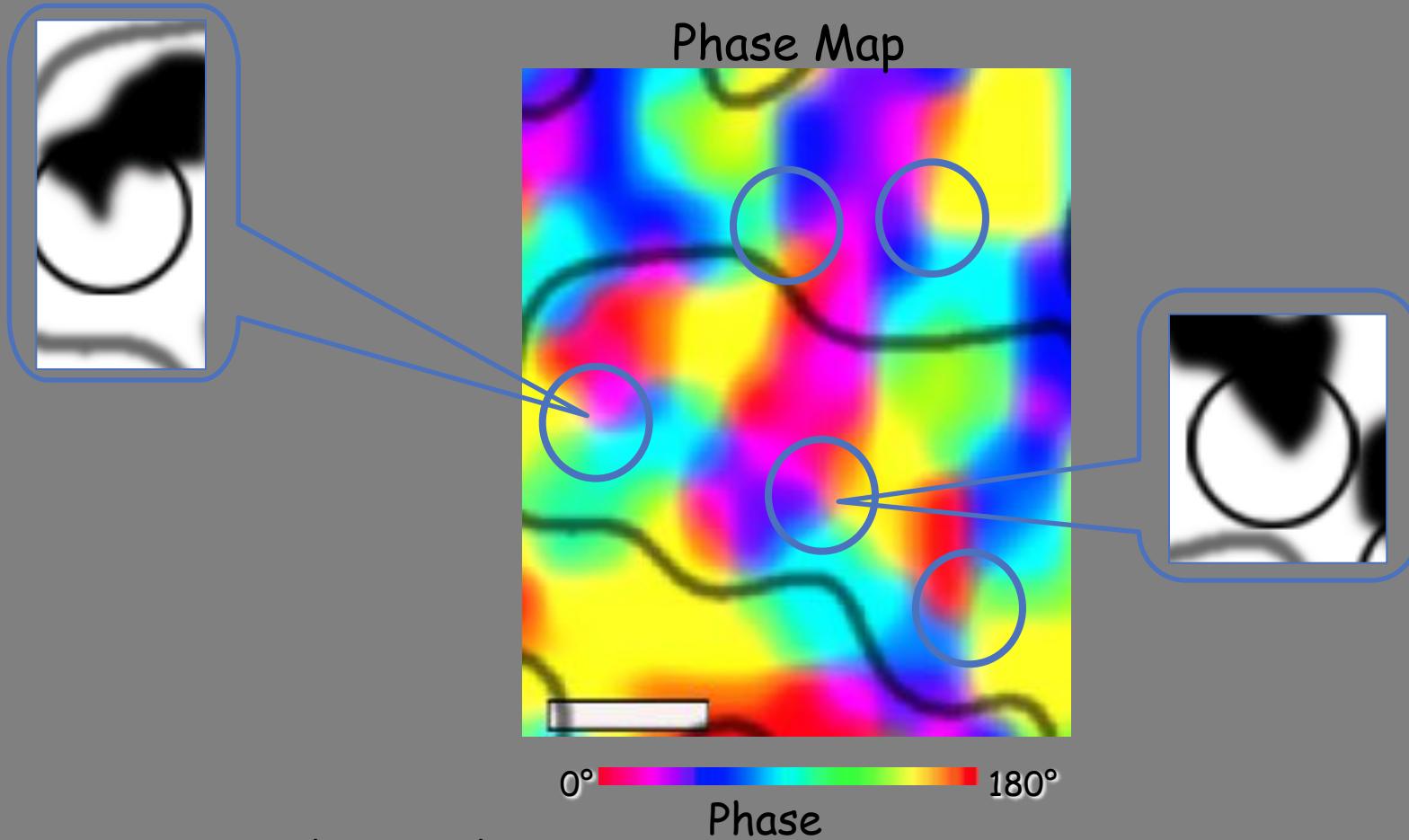


- Identical in size, orientation, and appearance to those obtained by optical imaging¹ and histology^{3,4}.

Menon et al.

- ¹Malonek D, Grinvald A. *Science* 272, 551-4 (1996).
³Horton JC, Hocking DR. *J Neurosci* 16, 7228-39 (1996).
⁴Horton JC, et al. *Arch Ophthalmol* 108, 1025-31 (1990).

Orientation Columns in Human V1 as Revealed by fMRI at 7T



Yacoub, Ugurbil & Harel
University of Minnesota / CMRR
HBM 2006: Thursday, June 15, 2006 at 9:30

Scalebar = 0.5 mm

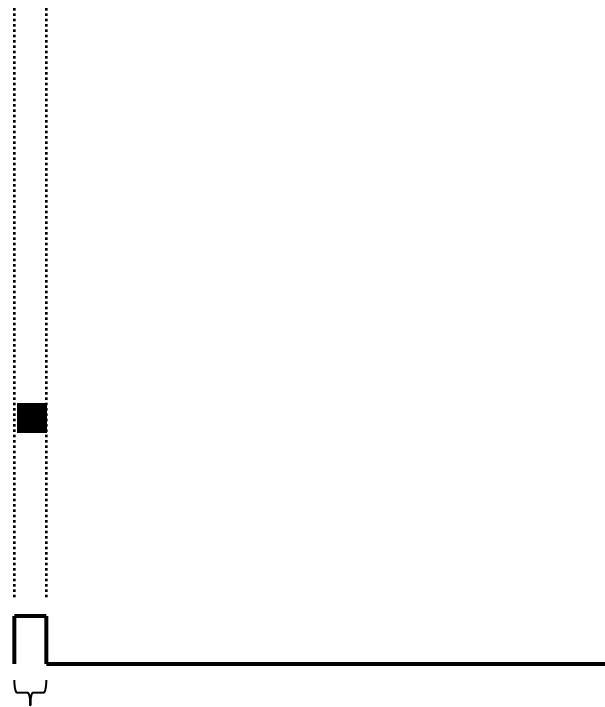
Temporal Resolution

The BOLD Signal

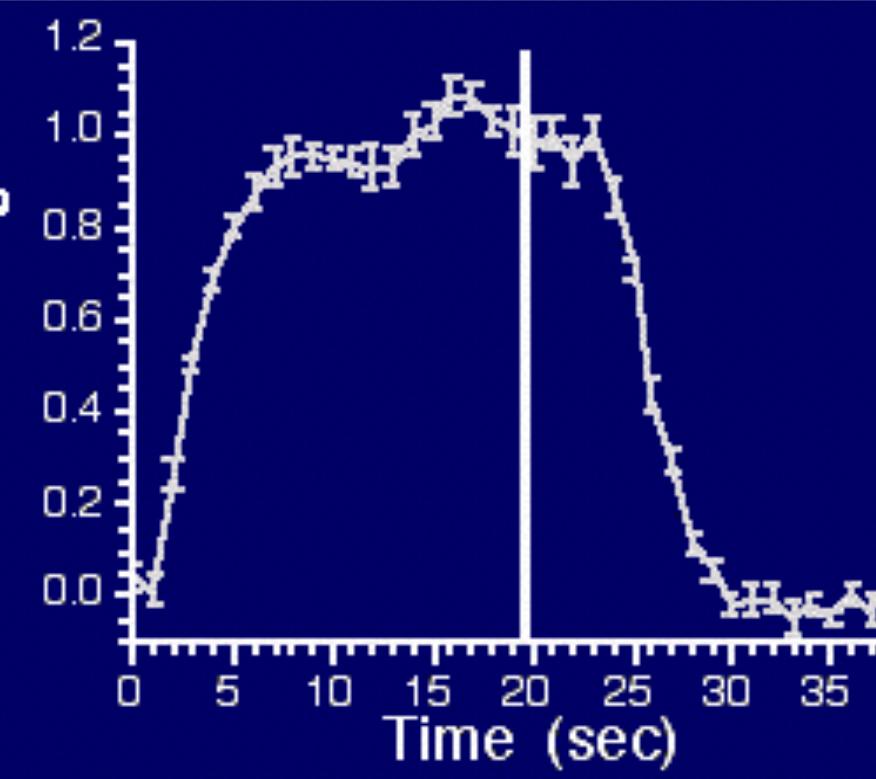
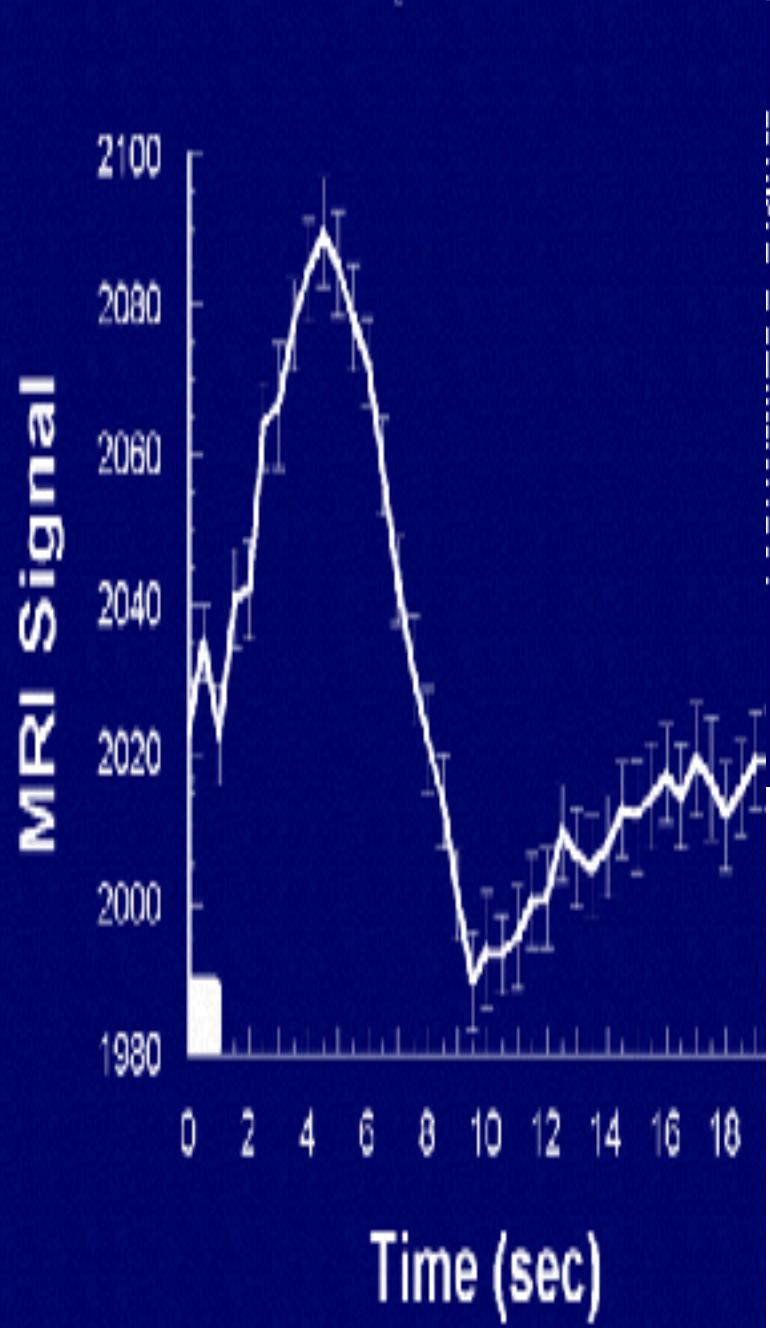
Blood Oxygenation Level Dependent (BOLD) signal changes



task

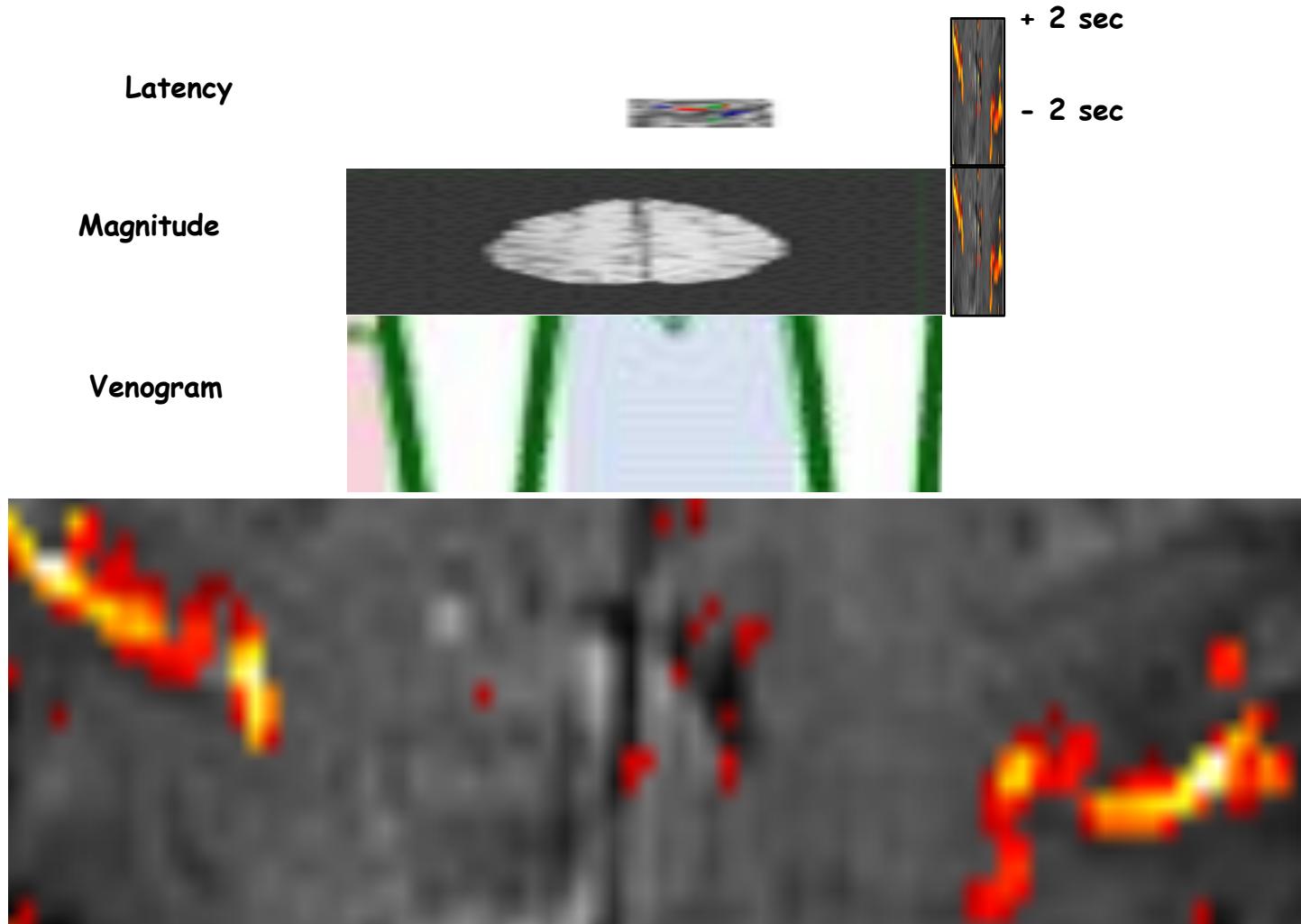


task



P. A. Bandettini, Functional MRI temporal resolution in "Functional MRI" (C. Moonen, and P. Bandettini., Eds.), p. 205-220, Springer - Verlag., 1999.

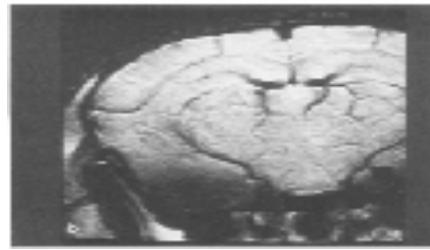
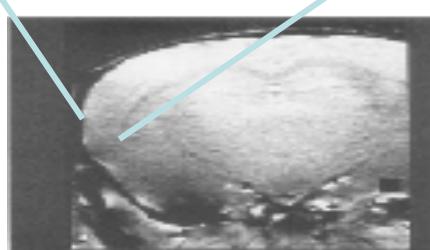
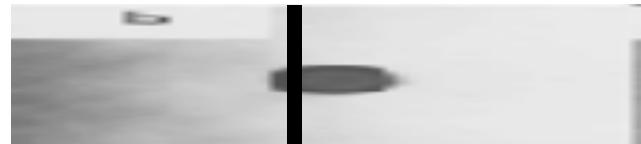
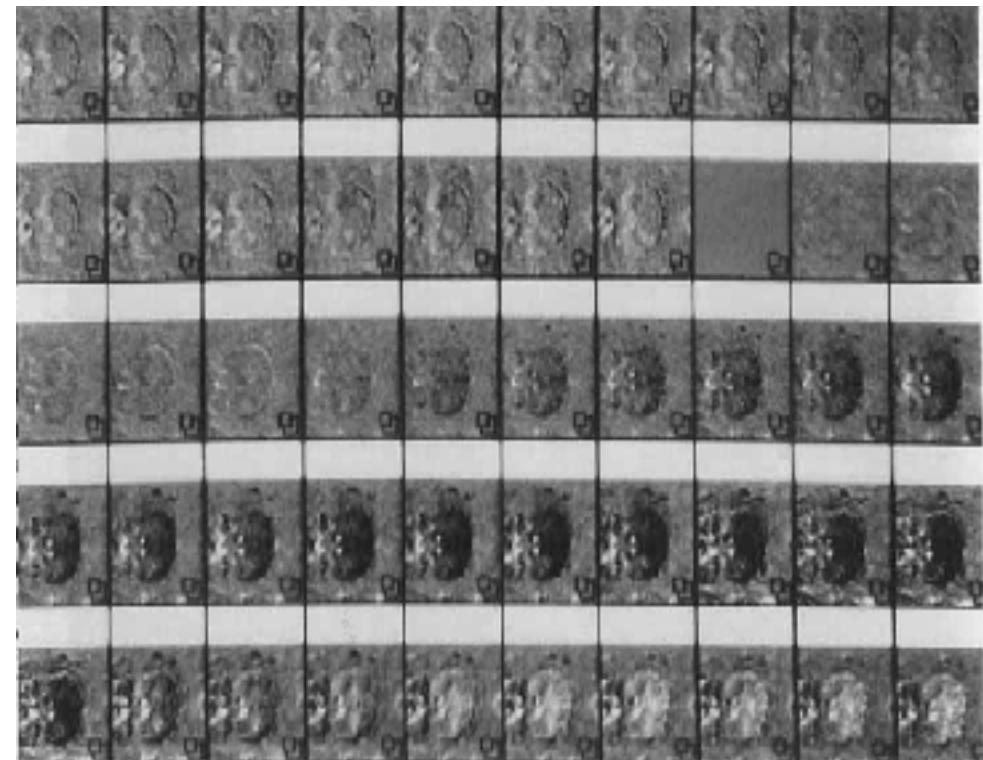
Latency Variation...



P. A. Bandettini, (1999) "Functional MRI" 205-220.

Word vs. Non-word

0°, 60°, 120° Rotation

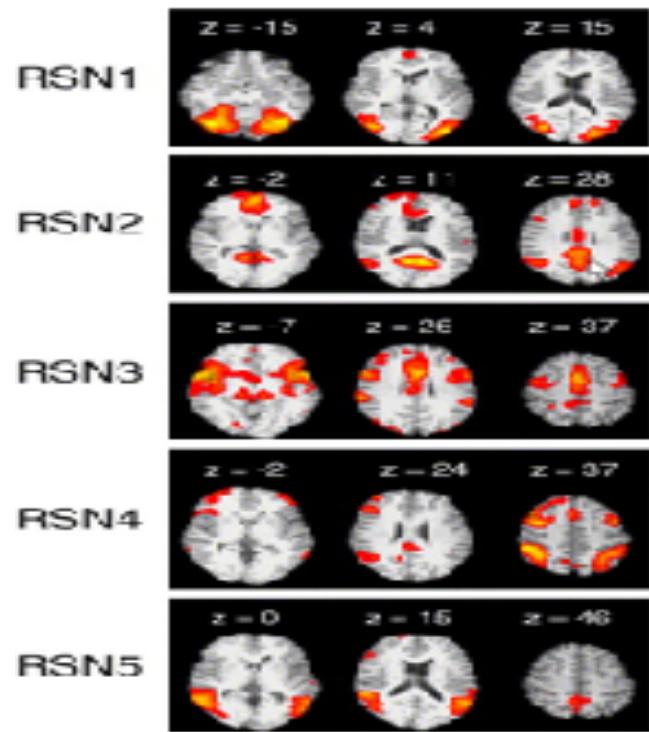
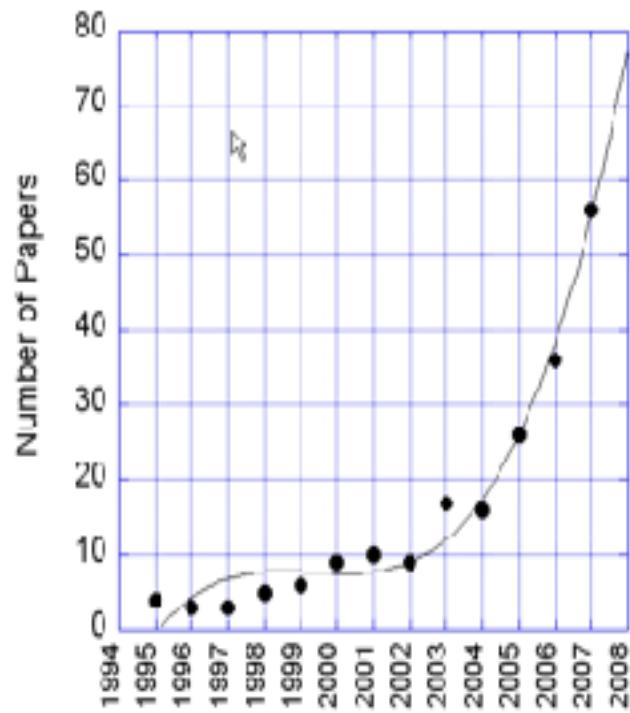


“Resting State”

Fluctuations

Hasson, et al (2004), *Science*, 303, 1634-1640

Resting State Correlations



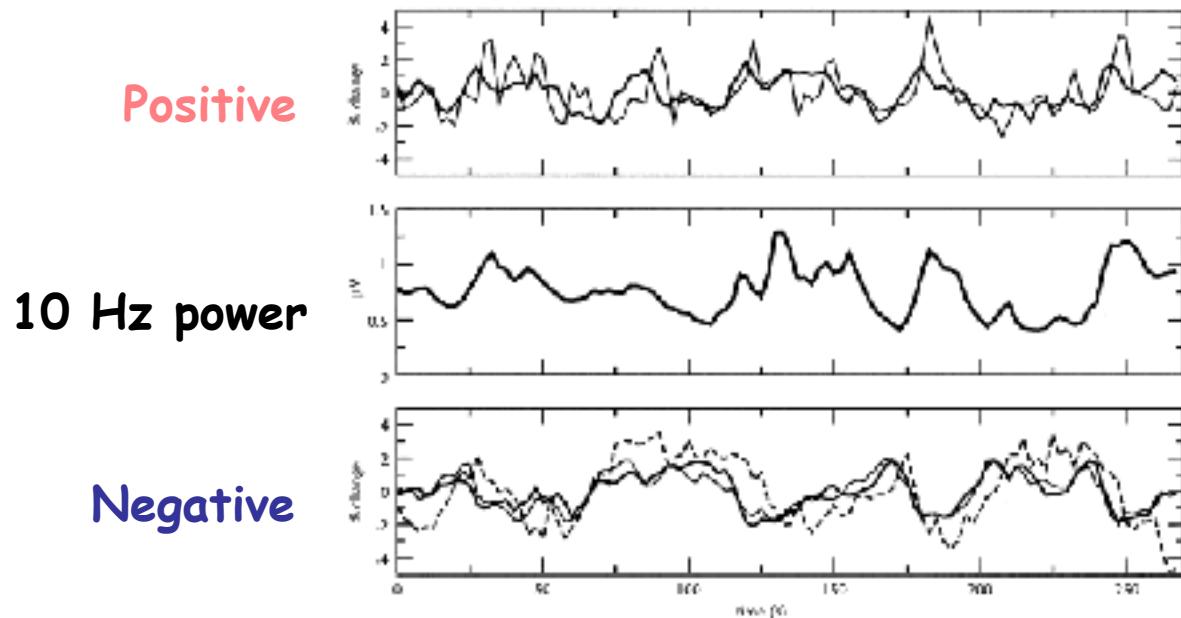
Activation:

correlation with reference function

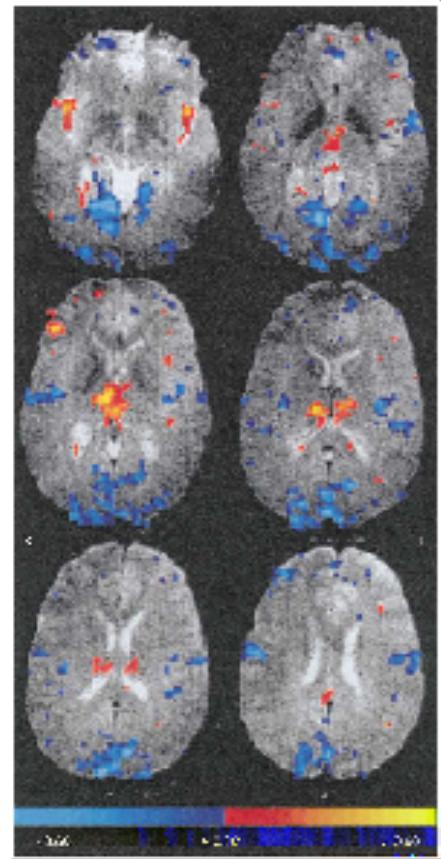
Rest:

seed voxel in motor cortex

BOLD correlated with 10 Hz power during "Rest"



Goldman, et al (2002), Neuroreport

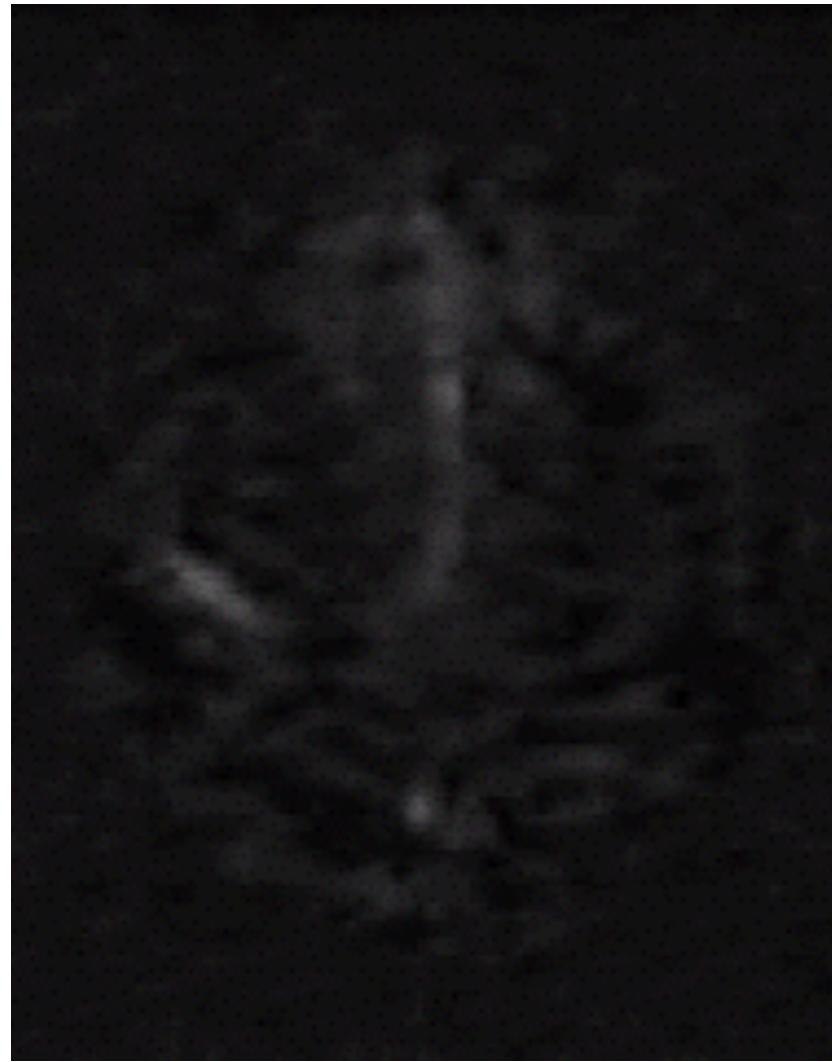


Resting state networks identified with ICA

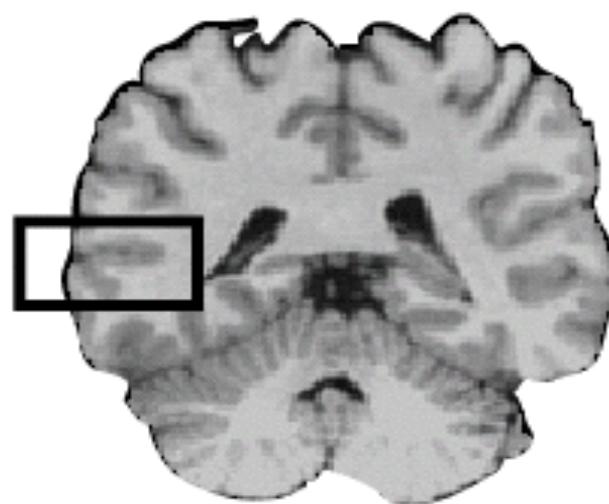
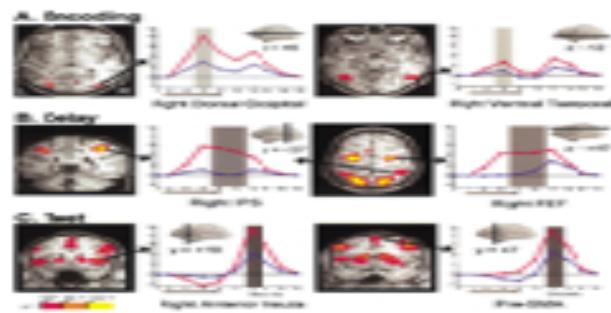
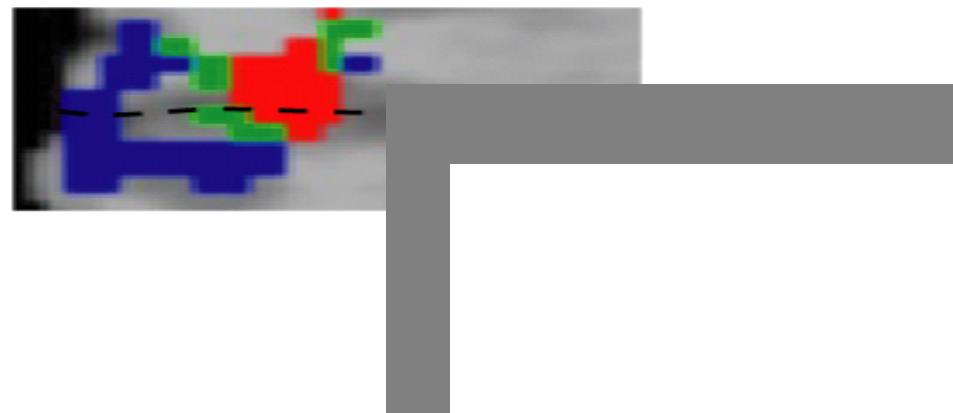
M. DeLuca, C.F. Beckmann, N. De Stefano,
P.M. Matthews, S.M. Smith, fMRI resting state
networks define distinct modes of long-distance
interactions in the human brain. NeuroImage, 29,
1359-1367

“Brain Reading”

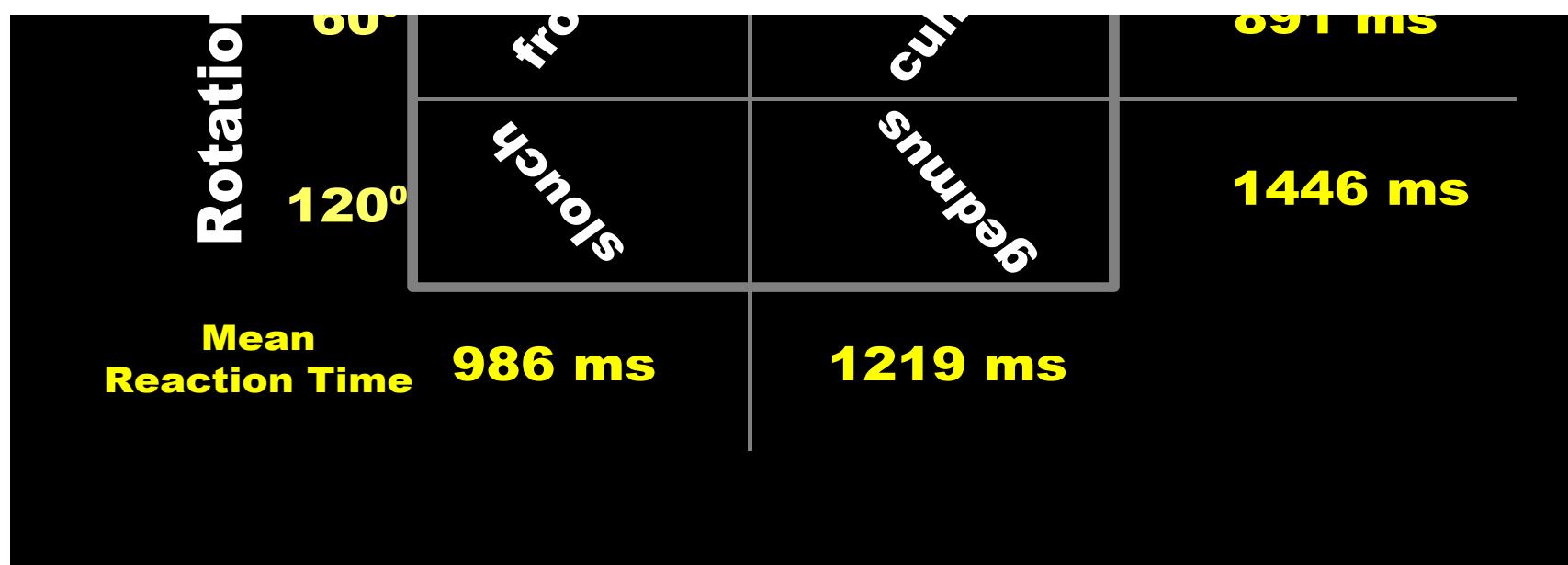
Methodology



Mapping \leftrightarrow “Reading”



Visual object categories distinguished by widely distributed inferotemporal activity pattern



Haxby et al. (2001)

Functional magnetic resonance imaging (fMRI) "brain reading":
detecting and classifying distributed patterns of fMRI activity
in human visual cortex

David D. Cox^{a,b,*} and Robert L. Savoy^{a,c}

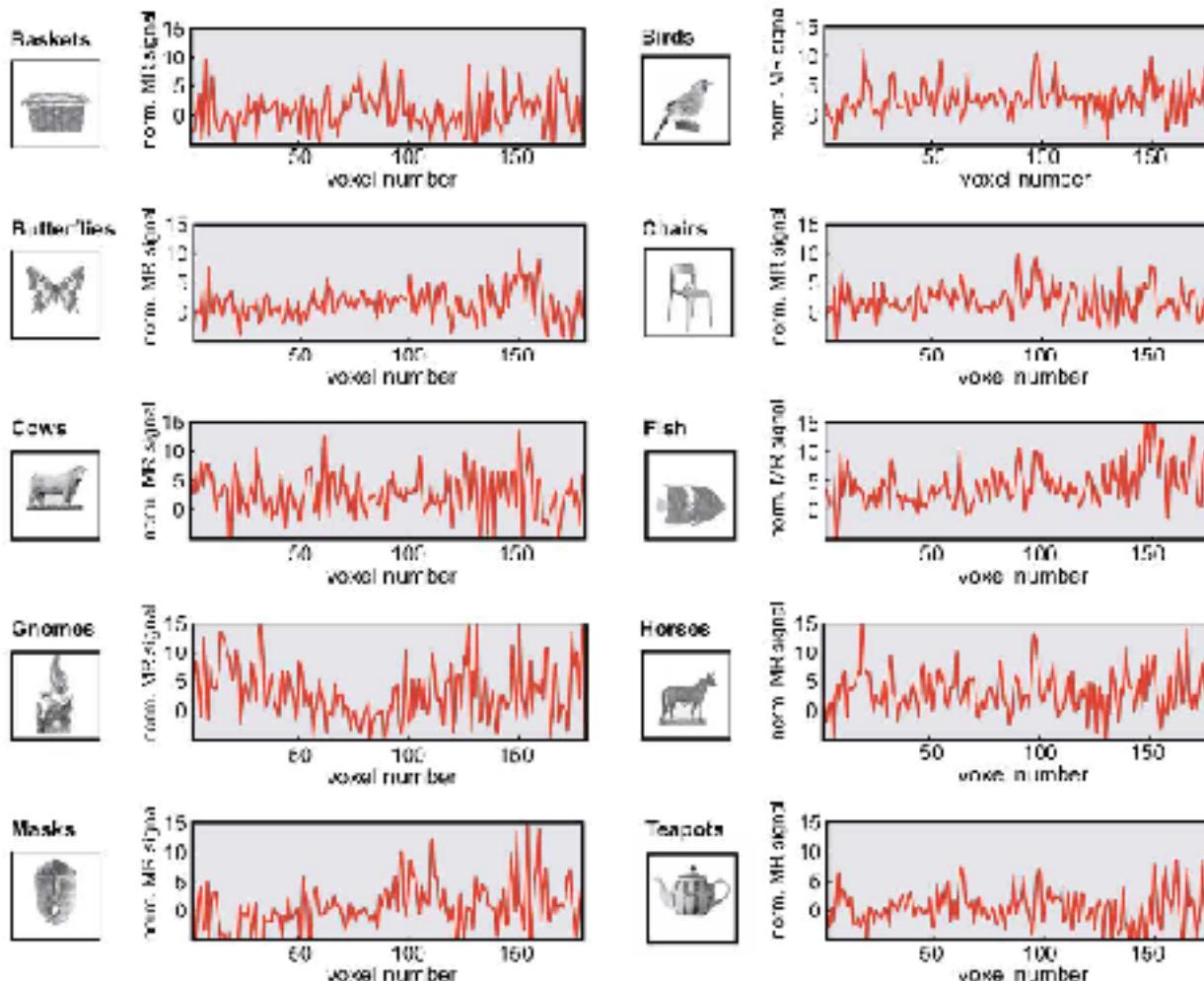
^a Broad Institute for Science, Cambridge, MA 02142, USA

^b McGovern Institute for Brain Research and ^c Division of Biological Imaging, Cambridge, MA 02139, USA

* Dept. Biostat., Tufts, P.O. Box 535, Lexington, MA 02426, USA

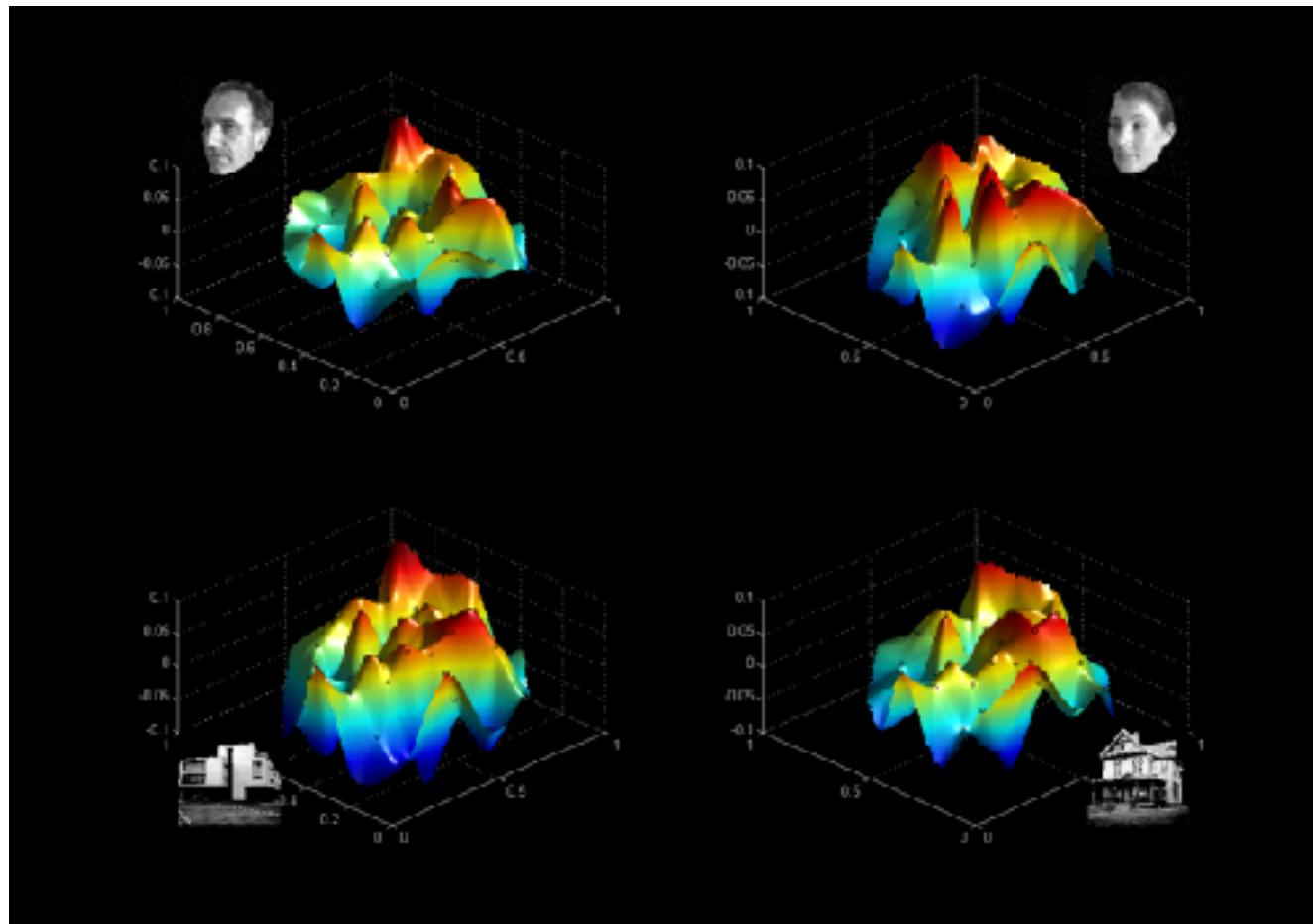
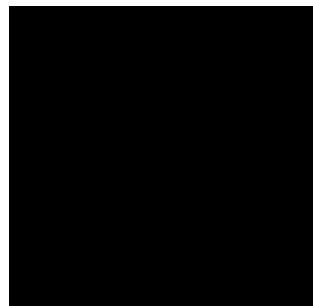
Received 15 July 2002; accepted 10 December 2002

NEUROIMAGE 19 (2): 261-270 Part 1 JUN 2003

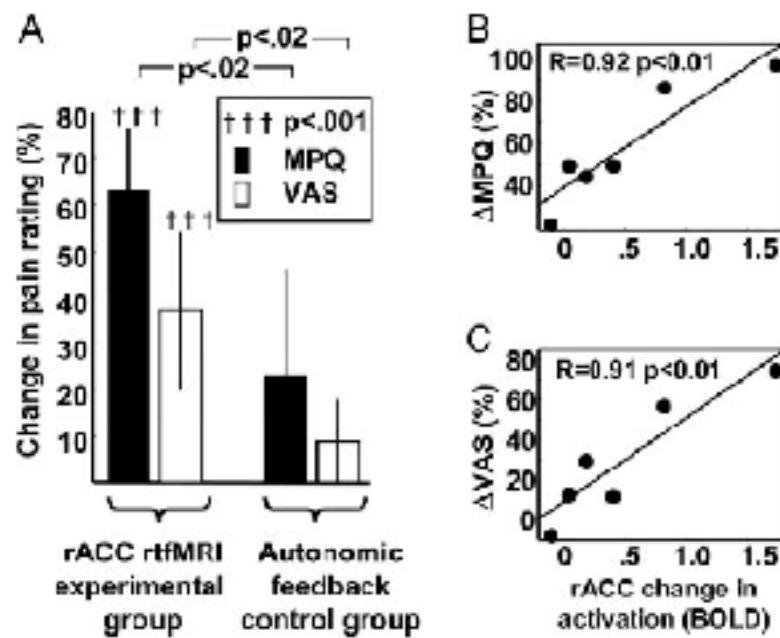
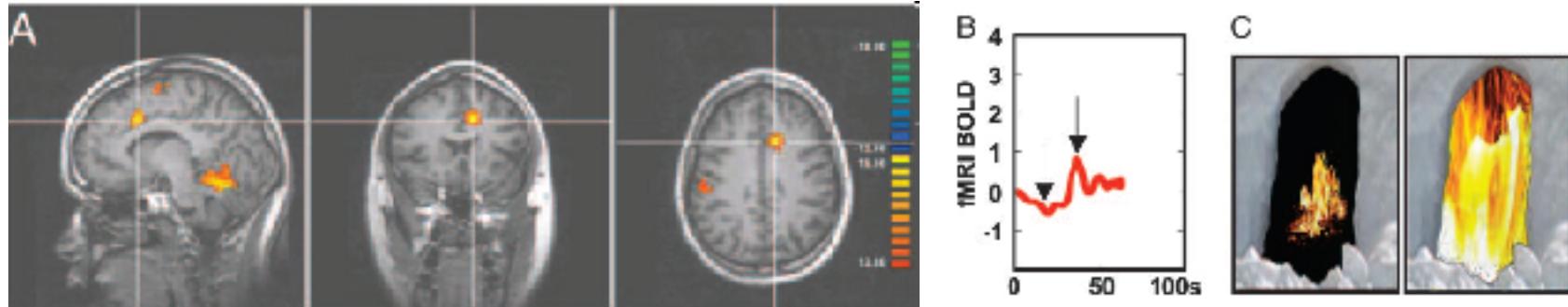


"searchlight" ROI

Multivariate analysis



Real time fMRI feedback to reduce chronic pain



Control over brain activation and pain learned by using real-time functional MRI, R. C. deCharms, et al. PNAS, 102; 18626-18631 (2005)

Current Uses of fMRI

Understanding normal brain organization and changes

- networks involved with specific tasks (low to high level processing)
- changes over time (seconds to years)
- correlates of behavior (response accuracy, performance changes...)

Clinical research

- correlates of specifically activated networks to clinical populations
- presurgical mapping
- epileptic foci mapping
- drug effects

Potential uses of fMRI

Complementary use for clinical diagnosis

- utilization of clinical research results

Clinical treatment and assessment

- drug, therapy, rehabilitation, biofeedback

Non clinical uses

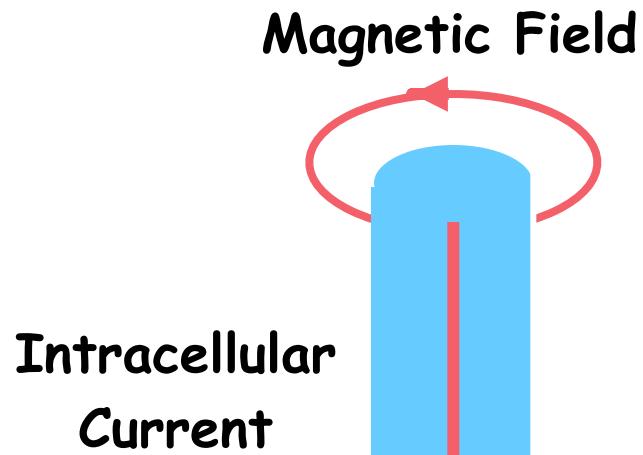
- complementary use with behavioral results
- lie detection
- prediction of behavior tendencies (many contexts)
- brain/computer interface

Section on Functional Imaging Methods & Functional MRI Facility Jan 19, 2007

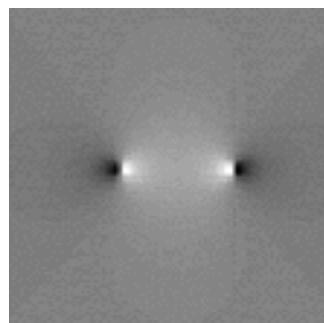
Back row: Wenming Luh, Niko Kriegeskorte, Rasmus Birn, Tyler Jones, Sean Marrett

Middle row: Jon West, Kay Kuhns, Anthony Boemio, Peter Bandettini, Joey Dunsmoor, Doug Ruff, Kevin Murphy

Front row: Dorian Van Tassel, Jerzy Bodurka, Adam Thomas, Marieke Mur, David Knight

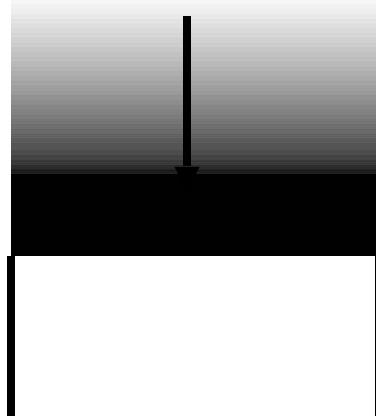


Surface Fields

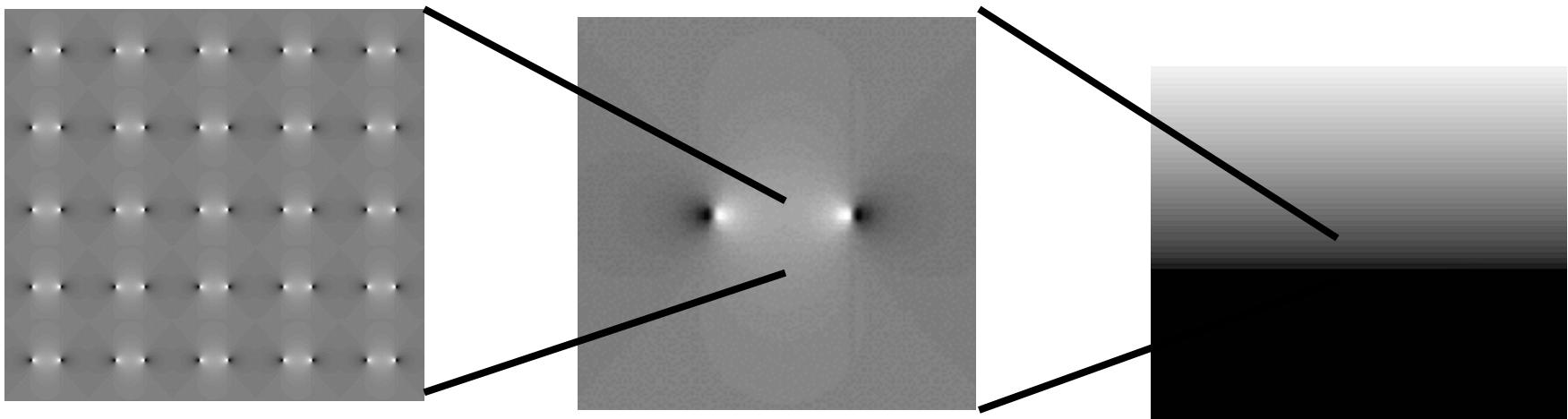


100 fT at on surface of skull

J.P. Wikswo Jr et al. J Clin
Neurophys 8(2): 170-188, 1991



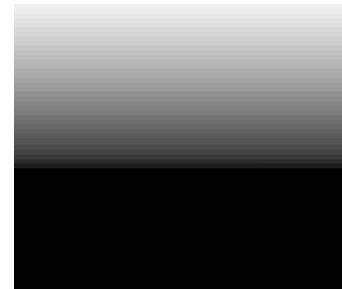
Surface Field Distribution Across Spatial Scales



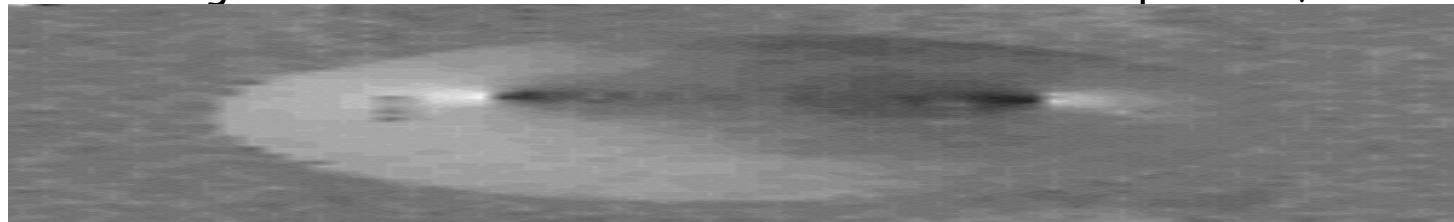
Adapted from: J.P. Wikswo Jr et al.
J Clin Neurophy 8(2): 170-188, 1991

Magnetic field associated with a bundle of dendrites

Because $B_{MEG} = 100\text{ fT}$ is measured by MEG on the scalp

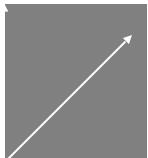
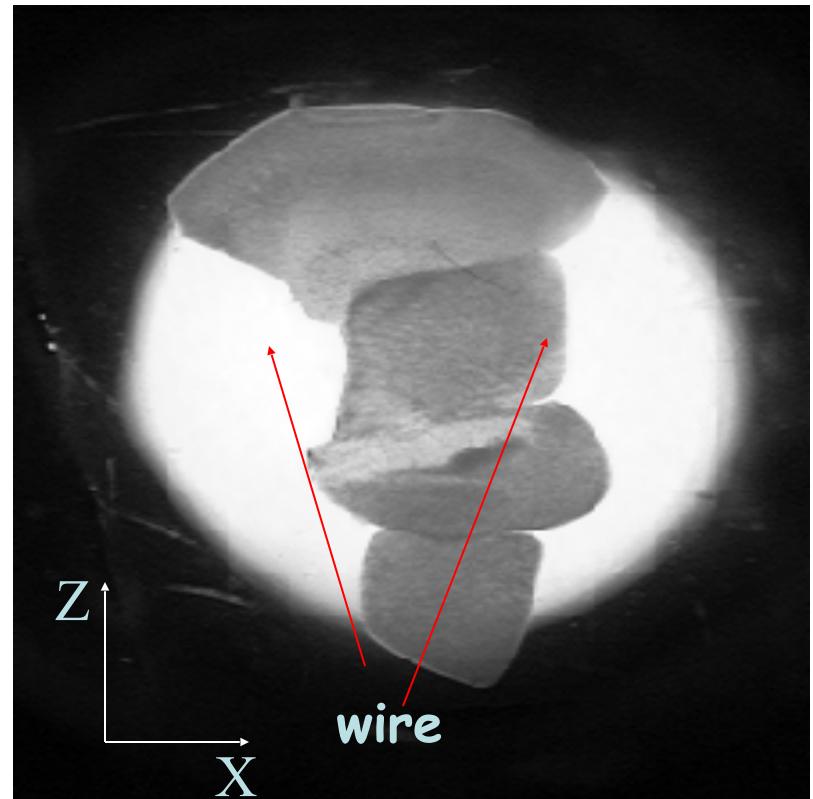
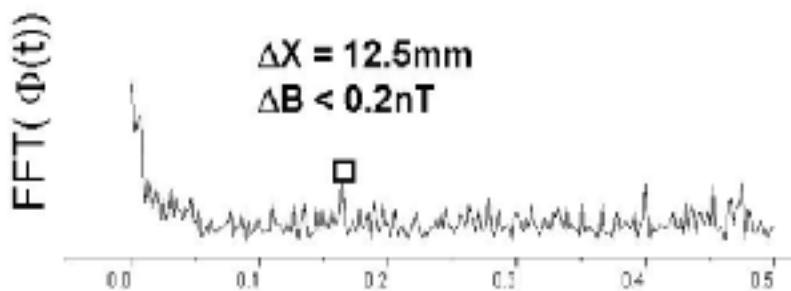
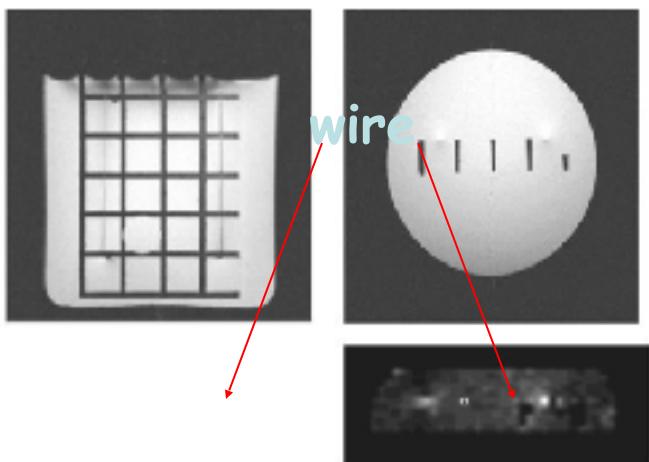


at least 50,000 neurons (0.002 fT (per dendrite) $\times 50,000 = 100\text{ fT}$), must coherently act to generate such field. These bundles of neurons produce, within a typical voxel, 1



$$B_{MRI} \approx 0.2\text{nT}$$

Current Phantom Experiment

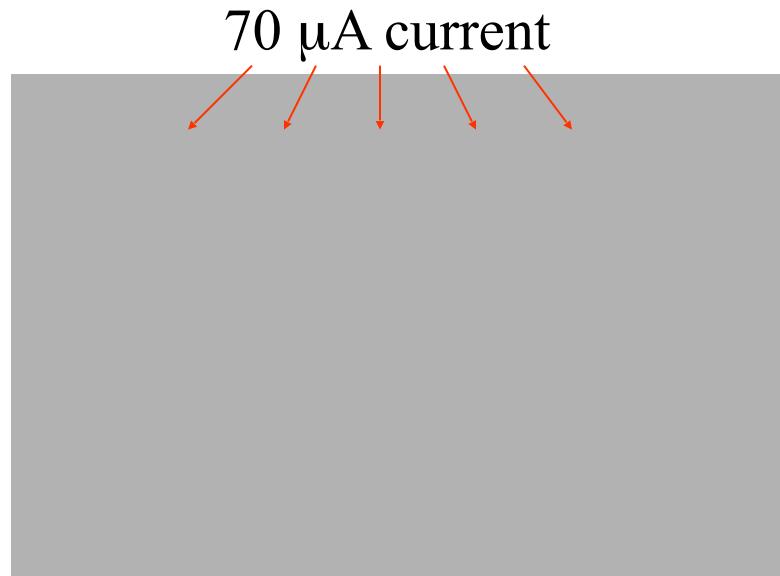


calculated $B_c \parallel B_0$

Measurement



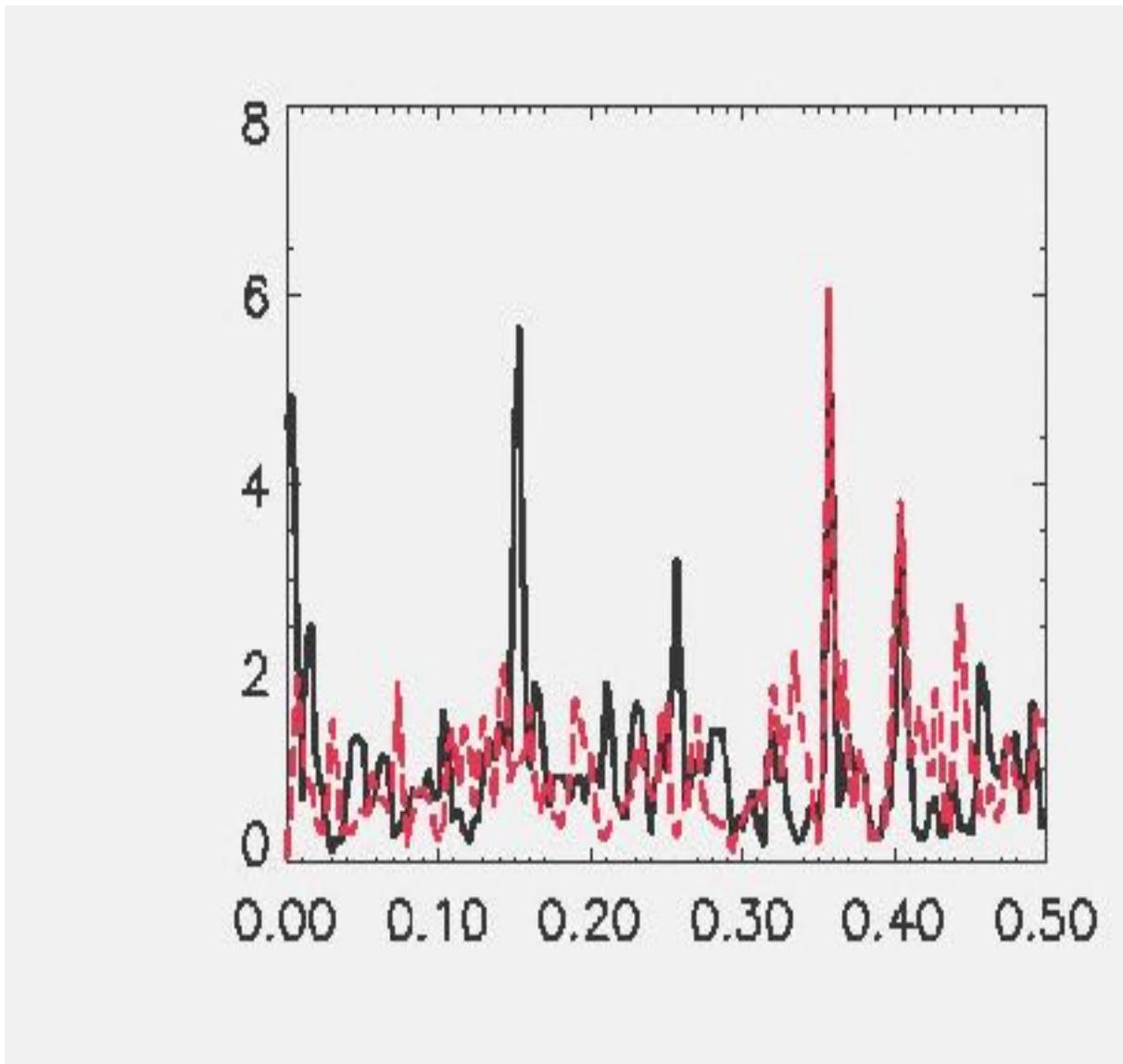
$$\Delta\phi \approx 20^\circ$$



Single shot GE EPI

Correlation image

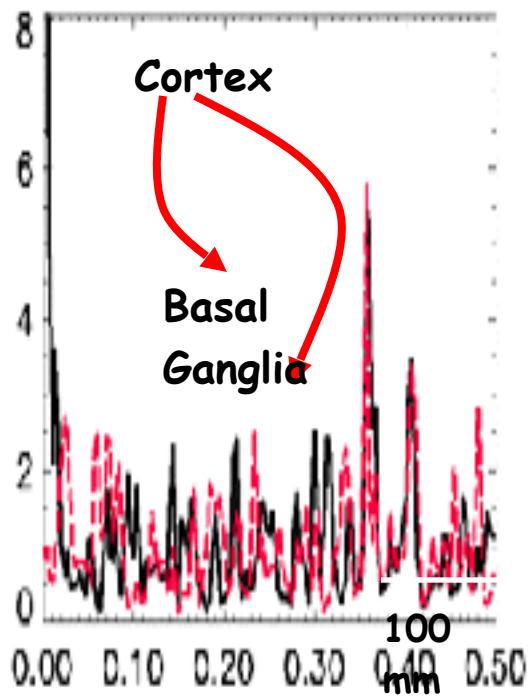
J. Bodurka, P. A. Bandettini. Magn. Reson. Med. 47: 1052-1058, (2002).



J. Bodurka, P. A. Bandettini. Magn. Reson. Med. 47: 1052-1058, (2002).

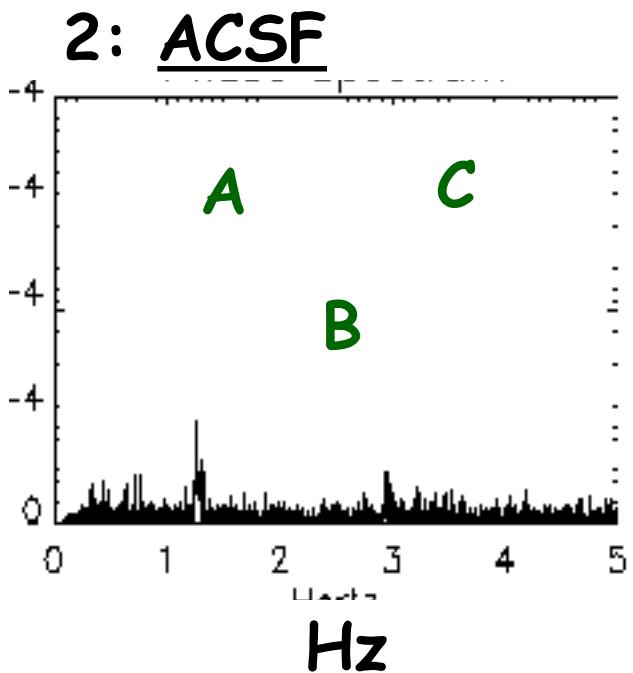
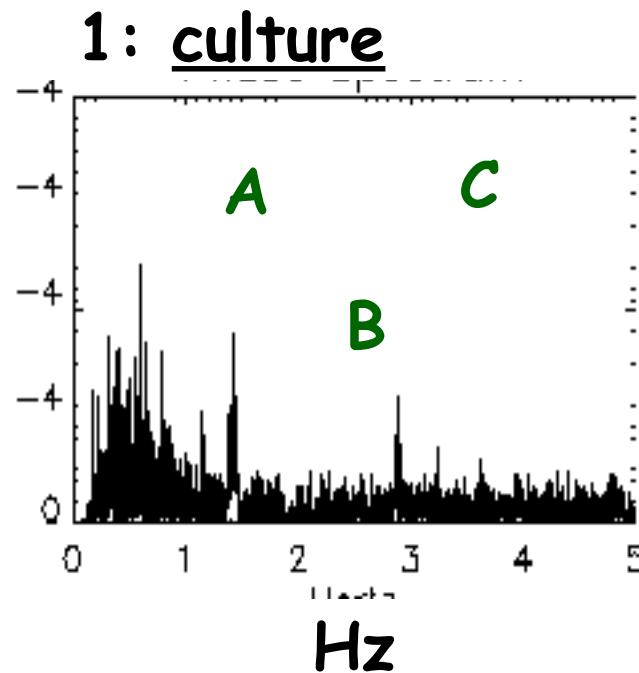
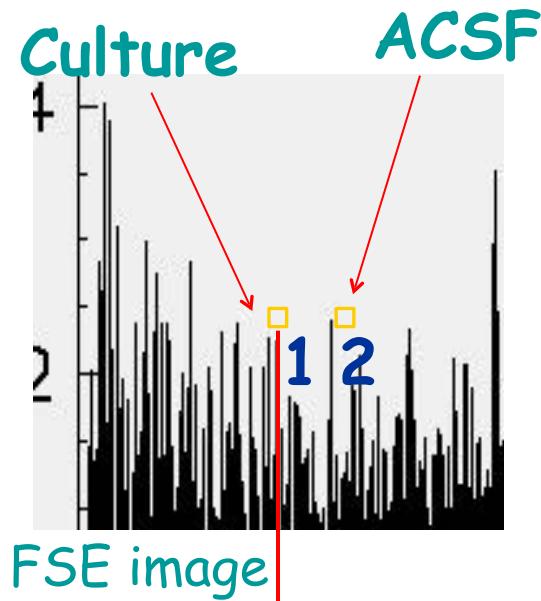
in vitro model

Organotypic (no blood supply or hemoglobin traces) sections of newborn-rat somato-sensory Cortex & Basal Ganglia



- Size: in-plane:~1-2mm², thickness: 60-100μm
- Neuronal Population: 10,000-100,000
- Spontaneous synchronized activity < 2Hz
- Epileptiform activity
- Spontaneous beta freq. activity (20-30Hz)
- Network Activity Range: ~ 0.5-15μV

3 Tesla data



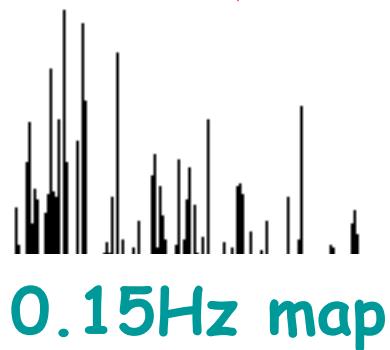
Active condition: black line

Inactive condition: red line

A: 0.15 Hz activity, on/off frequency

B: activity

C: scanner noise (cooling-pump)



7 Tesla data

TTX

Power decrease between PRE
& TTX EEG : ~ 81%

Decrease between PRE &
TTX MR phase: ~ 70%

Decrease between PRE &
TTX MR magnitude: ~ 8%

N. Petridou, D. Plenz, A. C. Silva, J. Bodurka, M. Loew, P. A.
Bandettini, Proc. Nat'l. Acad. Sci. USA. 103, 16015-16020 (2006).