On the static and dynamic features of edge time series



Time (seconds)

Joshua Faskowitz¹, Tyler Morgan¹, Daniel A. Handwerker¹, Javier Gonzalez-Castillo¹, Peter A. Bandettini^{1,2}

> ¹ Section on Functional Imaging Methods, ² Functional Magnetic Resonance Imaging Core Facility, National Institute of Mental Health, Bethesda, USA



Introduction

- Functional magnetic resonance imaging (fMRI) has repeatedly shown that BOLD signals will fluctuate across the cortex during task-free conditions
 - Fluctuating regions are often compared using **Pearson correlation**
 - Taking correlation between all region pairs forms a correlation, i.e., *functional connectivity*, matrix.
- Measuring the dynamic nature of correlations is increasingly popular; can reveal connectivity states⁵ and transients¹¹
- Edge time series^{3,16} render connectivity dynamics at the temporal resolution of the input time series
 - Recently, it has been shown that features of edge time series can be partially explained with features of static correlation^{9,12,13}.
- Here we further explore the relationship between static versus dynamic edge time series features.



Figure 2. By generating a toy system of 20 node time series with a planted covariance structure, we observe that modularity affects the maximum edge time series amplitude. a) Example matrices produced by the stochastic blockmodel, at different concentrations, which result in different modularity values (b) based on Potts model with a gamma of 1. c) After generating 200 synthetic matrices, time series, and subsequently edge time series for each network, the room-sum-square (RSS) of the edge time series are taken; more extreme RSS produced, as indicated by the red line, by more modular structures, as predicted and expected based on previous studies^{13,14} which discussed dependency of "events" on modularity or a



• Average edge time series \rightarrow Pearson's *r*

• Given this mathematical connection, what other relationships exist between time-average correlation and what we read out from edge time series?

Methods

Simulated data

- Time series generated with a 2-state Markov chain, convolved with a canonical HRF for five-second stimulus and bandpass filtered (0.008-0.08 Hz)
- Target covariance patterns were enforced on randomly generated and uncorrelated channels by projecting the data onto the axes of the eigen-decomposed covariance¹⁰
 - Using this method, we can control coupling (i.e., correlation) between two channels
- Randomly generated target covariance using the stochastic block model¹ a generative network model that allows for planted community structure with parameterized weight and edge existence

Real data

- Human Connectome Project resting-state data (0.72 TR, 1200 TRs, ~15 mins)
- Minimally pre-processed⁴: motion, distortion, bandpass, first/last 50 TRs discarded
- Nuisance regressed using aCompCor² components (5 WM, 5 CSF) and 24 motion parameters. Time series constructed by averaging vertex data within 200 node of Schaefer parcellation¹⁵, at each time point, using **Connectome Workbench**

• Edge time series

- Computed via the element-wise product of two z-scored time series; sum of which is correlation
- RSS: root of the sum of squares of all edge time series magnitudes, taken at each time point

relatively large leading eigenvector of the covariance matrix; max RSS: grey line, mean of max RSS: red dotted line

0.2



Figure 3. After increasing amount of principle components removed from time series data, binning patterns and RSS ETS change. a) RSS % bins were used demarcate data to construct 10 matrices & each matrix was compared to time-averaged connectivity, at each level of components removed b) ETS RSS as a matrix, showing how pattern of high amplitude events changes as function of variance removed c) Unperturbed ETS RSS d) Normalized ETS RSS at varying levels of perturbation, distinguished by color map; because generating ETS involves z-scoring, data with many components removed (>100) produce similar RSS magnitude as less perturbed,



Results



Figure 4. Applying randomization that preserves static covariance can still change edge time series phenomena. a) ETS RSS time series from an HCP resting-state scan, with varying levels of randomization applied (100 surrogate time series, as colored lines), according to the number of probabilistically sampled frequencies that were phase-shifted⁸; shift applied to all channels equally, maintaining original covariance pattern b) Transition probability matrices⁷ derived from ETS and surrogate data; based on t and t+1 transitions for each node, where affiliation is dictated by max. ETS magnitude at each time point c) Original vs. surrogate data transition probability values compared, demonstrating that even a slight perturbation to data, with time-averaged covariance held constant, causing between-system changes; suggests target for future ETS applications, not tethered to time-averaged covariance.

Figure 1. Using simulated data with parameterized coupling, we observe relationship between the similarity of node time series and the amplitude of edge time series. a) Example time series simulation for one channel using two-state Markov chain (blue) that is subsequently convolved with the HRF and bandpass filtered (green); 1000 time points generated b) Individual channels (n=200) adhere to bandpass filter (vertical red lines), whereas the ETS generation induces higher/lower amplitudes c) The distance (Kolmogorov-Smirnov) between node and ETS power spectra is systematically modulated by coupling of two channels, with min. around 0.8 d) Maximum values of time series within a narrow range compared to (e), the maximum values of ETS; coupling values derived from 200 simulations at each of 100 coupling values (0-.99, 0.01 steps), denoted by green-yellow color map

References

- 1. Aicher, C., Jacobs, A. Z., & Clauset, A. (2015). Learning latent block structure in weighted networks. Journal of Complex Networks
- 2. Behzadi, Y.(2007). A component based noise correction method (CompCor) for BOLD and perfusion based fMRI. Neuroimage
- 3. Faskowitz, J. (2020). Edge-centric functional network representations of human cerebral cortex reveal overlapping system-level architecture. Nat. Neuro.
- 4. Glasser, M. F. (2013). The minimal preprocessing pipelines for the Human Connectome Project. Neuroimage
- 5. Gonzalez-Castillo, J. (2015). Tracking ongoing cognition in individuals using brief, whole-brain functional connectivity patterns. PNAS
- 6. Greenwell, S. (2021). High-amplitude network co-fluctuations linked to variation in hormone concentrations over the menstrual cycle. Net. Neuro.
- 7. Gutierrez-Barragan, D. (2022). Unique spatiotemporal fMRI dynamics in the awake mouse brain. Current biology
- 8. Handwerker, D. A. (2012). Periodic changes in fMRI connectivity. Neuroimage
- 9. Ladwig, Z. (2022). BOLD cofluctuation 'events' are predicted from static functional connectivity. NeuroImage
- 10. Laumann, T. O. (2017). On the stability of BOLD fMRI correlations. Cerebral cortex
- 11. Liu, X. (2013). Time-varying functional network information extracted from brief instances of spontaneous brain activity. PNAS
- 12. Matsui, T. (2022). On co-activation pattern analysis and non-stationarity of resting brain activity. NeuroImage
- 13. Novelli, L. (2022). A mathematical perspective on edge-centric brain functional connectivity. Nature communications
- 14. Pope, M. (2021). Modular origins of high-amplitude cofluctuations in fine-scale functional connectivity dynamics. PNAS
- 15. Schaefer, A., (2018). Local-global parcellation of the human cerebral cortex from intrinsic functional connectivity MRI. Cerebral cortex
- 16. Zamani Esfahlani, F. (2020). High-amplitude cofluctuations in cortical activity drive functional connectivity. PNAS

This research was made possible thanks to the support of the NIMH Intramural Research Program ZIA-MH002783. This work utilized the computational resources of the NIH HPC Biowulf cluster (hpc.nih.gov).

Checkout github.com/faskowit/ohbm23 for example code in MATLAB



- Here we probe time series and edge time series characteristics, to obtain a better understanding of how their features are related. We illustrate:
 - ETS do not respect bandpass filter of original data (Fig1b), and the similarity of time series modulates the magnitude of ETS (Fig1c-e); implicates role of correlation for high amplitude ETS
 - Higher modularity of a simulated system results in higher amplitude ETS RSS (Fig. 2)
 - Similarity of ETS RSS binned data to time-averaged data holds for intact data (Fig3), and relationship is diminished after removing variance via incomplete PCA reconstructions
 - Small perturbations to time series (Fig 4a) results in large dynamics changes (Fig4b,c), even if time-averaged covariance is kept constant by the randomization method
- Indeed, some features of the time series are sufficient to estimate ETS properties¹³—notably those ETS properties that collapse across time, such as edge community similarity³ or the distribution of high-amplitude events into specific bins⁹.
 - Suggests that future work on edge time series should explore dynamics using the fine-grained precision that ETS can offer; opportunity for state-based analyses^{6,7}
 - Additional line of research will focus on comprehensively characterizing ETS channel properties (power/frequency, duty cycle, burstiness) to potentially distinguish if correlation appears different, for different functional relationships; i.e., investigating different fluctuation regimes across brain.